



# Toward Semi-autonomous Stiffness Adaptation of Pneumatic Soft Robots: Modeling and Validation

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## Introduction



Images from: "Soft robotics: Technologies and systems pushing the boundaries of robot abilities", Cecilia Laschi et al. (2016)



Soft Robotics Toolkit



K. Althoefer et. al. (2018)



# **Problem Definition**

The constant stiffness of the soft medical robots imposes a cap on their force transmission capacity.



Catheter positioning surgical robot Sensei ® X by Hansen Medical, USA – California

Limitation: They possess a pre-determined maneuverability and force transmission range.

**Dilemma in the usability of soft surgical robots:** Low stiffness is desirable for steerability; However, performing a specific task requires force transmission to the environment.



## Proposed Solution: Variable Stiffness Soft Robot



Stiffness of the soft robot can be decreased during the steering phase for high deformability and increased while performing tasks for high force transmission.



## **Related Studies**

• Soft robots  $\rightarrow$  Infinite DoFs  $\rightarrow$  Shape approximation methods:



Piecewise constant curvature (RJ Webster III et al., 2010)

(r, 0)



Shape as a set of small rigid segments with soft joints (RK. Katzschmann et al., 2019)



Cosserat rod model (Amir Hooshiar et al., 2020)



# Motivation:

Propose and validate a mechanistic model to investigate the effects of chamber pressure on the stiffness of the pneumatic-driven soft robots.

## **Contributions:**

- 1. Modeling the deformation of a single-chamber pneumatic driven soft flexure using Cosserat rod model,
- 2. Solution of the Cosserat model for a given tip force as an initial value problem (IVP),
- 3. Validation of the proposed model through experimentation,
- 4. Demonstrating the feasibility of stiffness modulation by changing the chamber pressure.



#### **Mechanistic Modeling: Kinematics**



A: cross-sectional area in its initial shape,

P: internal pressure,

F: external tip force,

s: arc parameter [0;L],

R(s): locally orthonormal frame,

 $\mathbf{p}(\mathbf{s})$ : position vector,

v(s): extension and shear strains along the backbone,u(s): bending and torsion strains along the backbone.

$$\mathbf{v}(s) = \mathbf{R}^T(s) \frac{\partial \mathbf{p}(s)}{\partial s}$$

$$\mathbf{u}(s) = \left(\mathbf{R}^T(s)\frac{\partial \mathbf{R}(s)}{\partial s}\right)^{\vee}$$



## Mechanistic Modeling: Conservation of Momentum



g= gravity vector



## Mechanistic Modeling: Constitutive Equations

Two-term Mooney-Rivlin (2MR) constitutive model for the material behavior of the soft robot for uniaxial elongation:

$$T_{11} = 2(c_{01} + \frac{c_{10}}{\lambda})(\lambda^2 - \lambda^{-1})$$

- $T_{11}$ : longitudinal nominal stress,
- $\lambda$ : longitudinal stretch,
- $c_{01}$  and  $c_{10}$ : material constants.

 Based on the Cosserat rod model, the linear elastic constitutive equations are:

$$\mathbf{n}(s) = \mathbf{R}(s)\mathbf{K}_{se}\Big(\mathbf{v}(s) - \mathbf{v}^{\star}(s)\Big)$$
$$\mathbf{m}(s) = \mathbf{R}(s)\mathbf{K}_{bt}\Big(\mathbf{u}(s) - \mathbf{u}^{\star}(s)\Big)$$

By substituting the derived shear and Hooke's
Moduli, the tangent stiffness matrices is:

$$\mathbf{K}_{se} = \operatorname{diag} \begin{pmatrix} E_{\circ}A & G_{\circ}A & G_{\circ}A \end{pmatrix}$$
$$\mathbf{K}_{bt} = \operatorname{diag} \begin{pmatrix} 2G_{\circ}I & E_{\circ}I & E_{\circ}I \end{pmatrix}$$



#### **Mechanistic Modeling: Solution**

> Runge-Kutta (RK4) method with a step-size of  $\delta_s = \frac{L}{100}$ 

 Dirichlet and Neumann boundary conditions at s = 0 that were formulated as:

$$\mathbf{p}(s)|_{s=0} = \begin{pmatrix} 0 & 0 & 0 \end{pmatrix}^{T}, \\ \mathbf{u}(s)|_{s=0} = \begin{pmatrix} 1 & 0 & 0 \end{pmatrix}^{T}, \\ \mathbf{R}(s)|_{s=0} = \mathbf{I}_{3\times 3}, \\ \mathbf{v}(s)|_{s=0} = \mathbf{0}. \end{cases}$$

Model parameters of the prototyped soft robot.

	Length	Outer Dia.	Inner Dia.	2MR Constants		Density
Parameter	L	$D_o$	$D_i$	$c_{01}$	$c_{10}$	$\rho$
	(mm)	(mm)	(mm)	(kPa)	(kPa)	$\left(\frac{g}{cc}\right)$
	85	12	3.5	277	-209	1.04



Deformation of the soft robot under its weight and a tip force of 30 mN in +z-direction with various chamber pressures.

## Mechanistic Modeling: Stiffness Surface

> Stiffness:

$$k = \frac{\partial ||\mathbf{F}||}{\partial ||\mathbf{p}(s = L)||} = k(F, P)$$



Variation of the soft robot's stiffness with internal pressure and tip force.



## Validation Study: Setup

- Pressure regulator: ITV0010-3UML, SMC, Tokyo, Japan
- Desktop CNC
- RGB-D camera: D435i, Intel Corp., CA, USA
- Force Sensor: ATI Industrial Automation, F/T Sensor, Mini40

## Validation Study: Protocol

- Pressure range: 0 20 kPa
- ➢ Tip displacement: 0 − 15 mm
- > Force range: 0 89 mN





#### Validation Study: Results

Stiffness of the soft robot increased from 3.4  $\frac{mN}{mm}$ (P=0 kPa) to 5.9  $\frac{mN}{mm}$  (P=20 kPa) indicating a 74% pressure-stiffening effect.

Pressure	Tip Force	Tip Displacement		Displacement Error		Stiffness	
(kPa)	(mN)	Model (mm)	Reference (mm)		Absolute (mm)	Relative (%)	(mN/mm)
0	51	14.4	15		0.6	3.4%	3.4
4	64	14.3	15		0.7	4.7%	4.3
12	73	13.9	15		1.1	7.3%	4.9
20	89	13.7	15		1.3	8.7%	5.9

Comparison of the model results with experiments.







#### **Conclusion:**

- > IVP with homogeneous Neumann and Dirichlet boundary conditions,
- Comparison of the theoretical findings with experimental results for tip displacement and stiffness showed similar trends with a maximum error of 8.7%,
- The findings confirmed the feasibility of stiffness adaptation through chamber pressure regulation.

#### Future works:

- Exploiting the pressure-stiffening phenomenon for stiffness adaptation of soft surgical robots during interventional procedures,
- > Effects of presence of multiple chambers for directional stiffening,
- Feasibility of position-stiffness hybrid control through tendon-pneumatic actuation.





# **Thank You**

