

A data-driven approach to feature space selection for robust micro-endoscopic image reconstruction

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Context

Multi-photon microendoscopy allows real-time imaging of cellular-level morphology with high contrast, high penetration depth, minimal photo-toxicity and limited sensitivity to the diffusion of biological materials [Duc15]. However, the acquisition of large tissue areas requires a process of multi-view reconstruction from a sequence of low-field-of-view images. Noise, illumination changes and geometric distortions induced by hand motion and optics are making the visual matching of said images a challenging task for reconstruction. In this article, we propose a new on-line image feature space selection strategy for displacement field estimation.

Visual matching using convex optimization

Given a small enough deformation or hand displacement between two consecutive images, we want to identify a geometric transform $\mathbf{W}(\mathbf{x}, \boldsymbol{\theta}_t)$ such that:

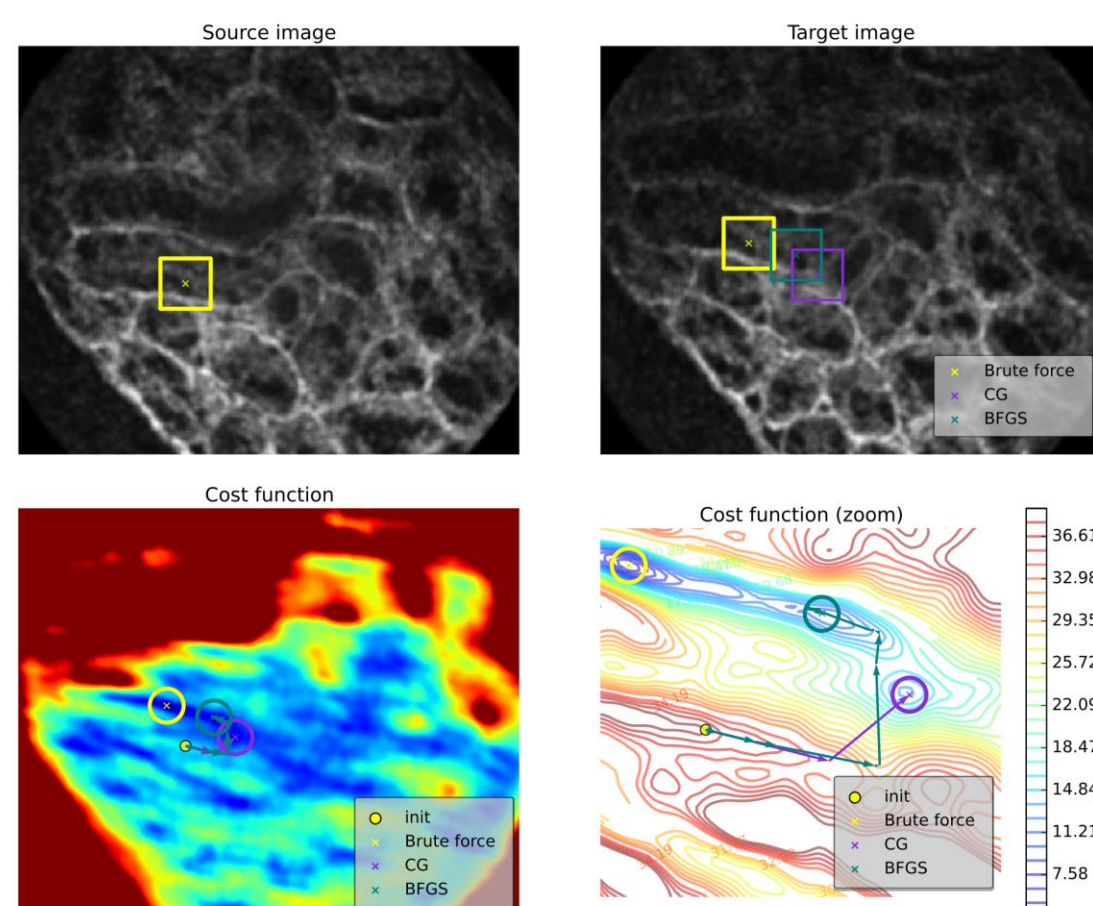
$$I(\mathbf{x}, t + \partial t) = I(\mathbf{W}(\mathbf{x}, \boldsymbol{\theta}_t), t)$$

Image registration then consists in estimating a set of parameters $\boldsymbol{\theta}_t$ which satisfy this equation *i.e.* :

$$\tilde{\boldsymbol{\theta}}_t = \arg \min_{\boldsymbol{\theta}_t} (\xi(\boldsymbol{\theta}_t))$$

$$\xi(\boldsymbol{\theta}_t) = \sum_{\mathbf{x} \in \mathcal{Y}} \|I(\mathbf{x}, t) - I(\mathbf{W}(\mathbf{x}, \boldsymbol{\theta}_t), t + \partial t)\|_2^2$$

Where objective function $\xi(\boldsymbol{\theta}_t)$ is considered convex and smooth enough to provide a good estimation of $\boldsymbol{\theta}_t$. However it is not the case with our microendoscopic image data :



Data-driven feature space selection

Suppose there exists a set of image feature spaces $\mathbf{F}(\mathbf{x}, t)$ for which $\xi(\boldsymbol{\theta}_t)$ is actually convex. We could use a linear combination ($\boldsymbol{\beta}$ -weighted) of said features to define a new cost function:

$$\hat{\boldsymbol{\theta}}_t(\boldsymbol{\beta}) = \arg \min_{\boldsymbol{\theta}_t} (\xi_{\boldsymbol{\beta}}(\boldsymbol{\theta}_t)) = \hat{\boldsymbol{\theta}}_t$$

$$\xi_{\boldsymbol{\beta}}(\boldsymbol{\theta}_t) = \sum_{\mathbf{x} \in \mathcal{Y}} \|\boldsymbol{\beta}^T \cdot (\mathbf{F}(\mathbf{x}, t) - \mathbf{F}(\mathbf{W}(\mathbf{x}, \boldsymbol{\theta}_t), t + \partial t))\|_2^2$$

where $\hat{\boldsymbol{\theta}}_t$ are ground truth parameters recovered from brute-force search over the original image domain.

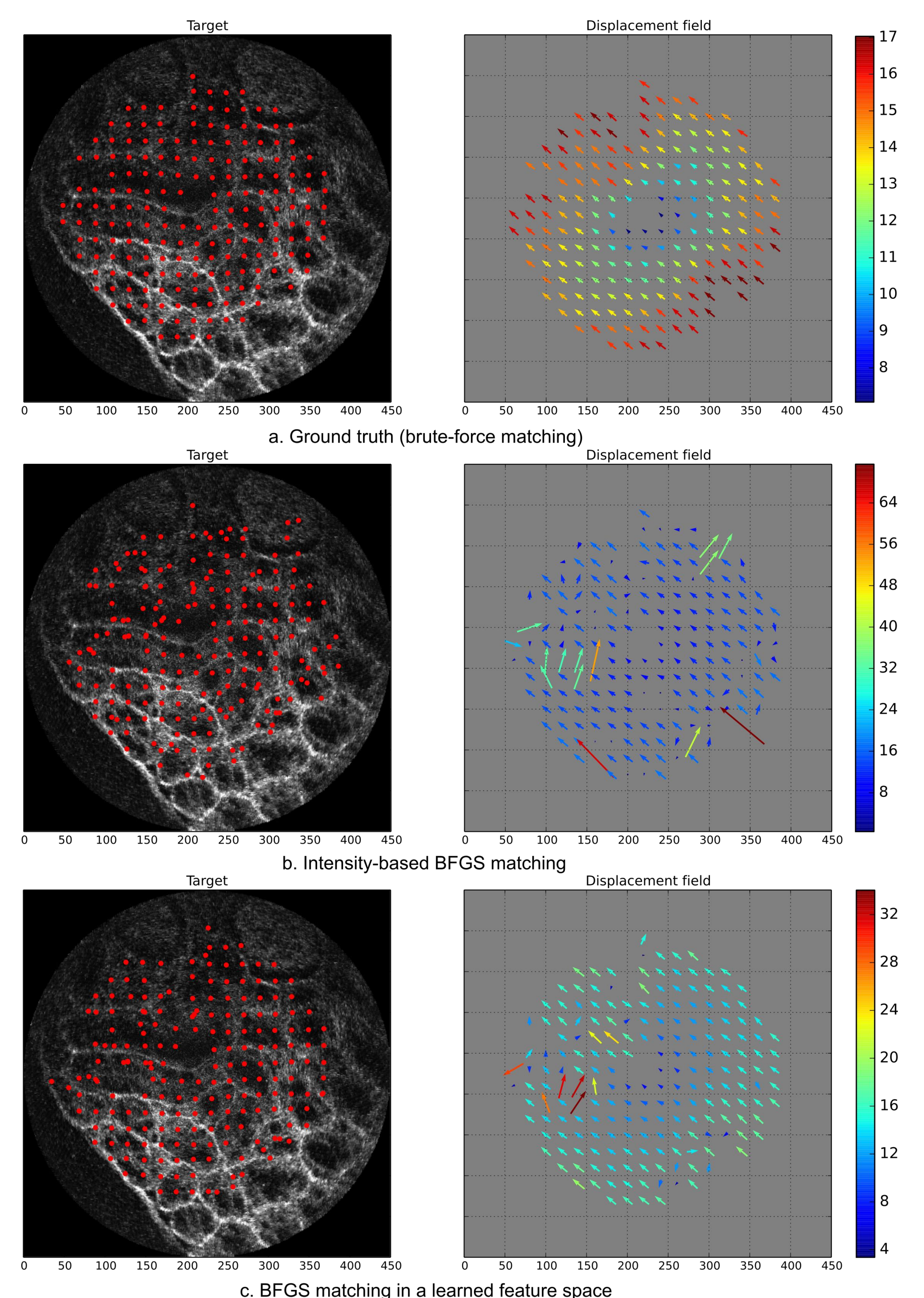
The estimation of feature weighting vector $\boldsymbol{\beta}$ is a key element of our method. We are looking for a sparse solution to reduce computation times and provide safety against redundant feature descriptions. Hence the addition of a L1-norm constraint:

$$\hat{\boldsymbol{\beta}} = \arg \min_{\boldsymbol{\beta}} \left(\alpha \|\boldsymbol{\beta}\|_1 + \sum_{t \in [0, t_0]} \|\hat{\boldsymbol{\theta}}_t - \tilde{\boldsymbol{\theta}}_t(\boldsymbol{\beta})\|_2^2 \right)$$

In practice the endoscope operator is required to capture a few images for ground truth generation, with brute-force matchings providing the algorithm with $\hat{\boldsymbol{\theta}}_t$ samples.

Experimental results

Data: 450x450 low-field images taken with a 250 μ m fiber endoscope. Image features : scale-variant polynomials and Gabor wavelets. Local optimization: BFGS algorithm.



Feature space	MSE	SD
Raw pixel intensity	12.67	± 19.40
Multi-scale polynomial, $\alpha = 0.1$	11.05	± 16.70
Multi-scale polynomial, $\alpha = 1.0$	10.37	± 14.57
Gabor wavelet basis, $\alpha = 0.1$	11.21	± 16.66
Gabor wavelet basis, $\alpha = 1.0$	11.05	± 16.70

Conclusion

- A new feature space selection method for displacement field estimation
- On-line learning of ground truth data from non-optimal global methods

[Duc15] Ducourthial et al (2015). Development of a real-time flexible multiphoton microendoscope for label-free imaging in a live animal. Scientific reports, Nature Publishing Group.