Cepstrum Coefficients Based Sleep Stage Classification

Emin Argun Oral

Electrical-Electronics Engineering Department Atatürk University Erzurum, TURKEY

November 14, 2017



Sleep is the resting state of the body External stimuli is weakened

Activities are reduced

Sleep Disorder

- May cause mental fatigue and stress, even psychiatric or mental illnesses, such as loss of consciousness
- Negative effect on person's professional and social life
- Important to monitor sleep deprivation and disorders

Polysomnography (PSG)

- Current method for the diagnosis and treatment of sleep deprivation and disorders
- Monitors changes during sleep, generally night time
- Simultaneous and continuous recording of neurophysiological, cardiorespiratory, other physiological and physical changes
- Signals obtained by PSG are classified (scored) by an expert for a diagnosis according to some predefined standards

Scoring

- Sleep staging (scoring) is typically performed manually
- Manual of sleep classification by Rechtschaffen and Kales (R&K)
 - widely used since 1968
 - sleep recordings are divided into 7 discrete stages
 - wakefulness, stage 1 (S1), stage 2 (S2), stage 3 (S3), stage 4 (S4), stage REM and movement time

American Academy of Sleep Medicine (AASM)

- defined in 2007, scoring rules and terminology of R&K are modified
- sleep recodings are divided into 5 discerete stages
- wake (W), NREM1 (N1), NREM2 (N2), NREM3 (N3) and stage REM (R)
- sleep stages S1 to S4 of R&K are referred to as NREM1 (N1), NREM2 (N2), NREM3 (N3)
- NREM₃ (N₃) slow wave sleep (SWS): reflecting combination of S₃ and S₄

Scoring / Classification

Scoring is the manual evaluation and labeling of PSG recordings

- An expert for evaluation
- Open to human errors
- Time consuming
- Use various physiological signals as well as multiple sensors
 - Causes the subject to move away from home environment to a hospital
 - Also feels uncomfortable for the use of multiple sensors and wires attached to his or her body during sleep
- Help of a computer using machine learning algorithms
- Automatic classification using single-channel EEG recordings has been widely preferred

Current Study

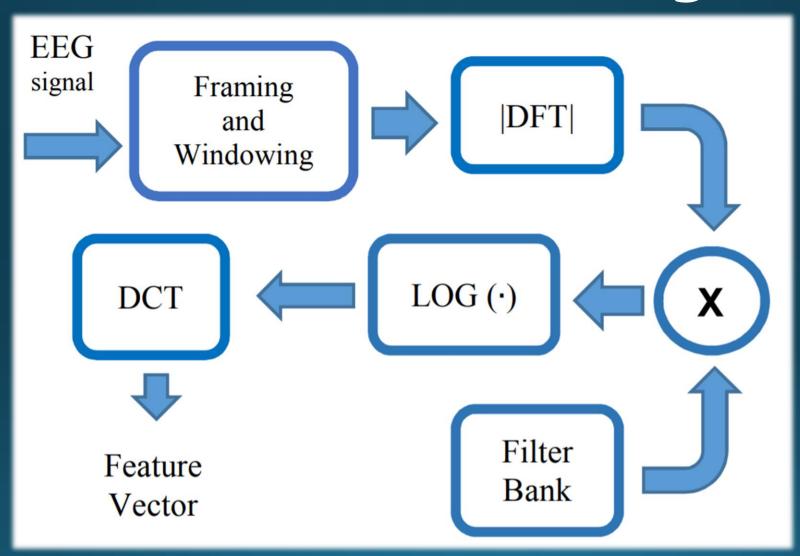
- Classification of sleep stages as wake, REM and NREM
- Single-Channel EEG signals
- Composed of two main steps
 - Feature Extraction
 - Classification
- Cepstrum coefficients are used in feature extraction
- Support Vector Machine (SVM) is used in classification

Feature Extraction

Filterbank based cepstrum coefficients are used to form feature vector

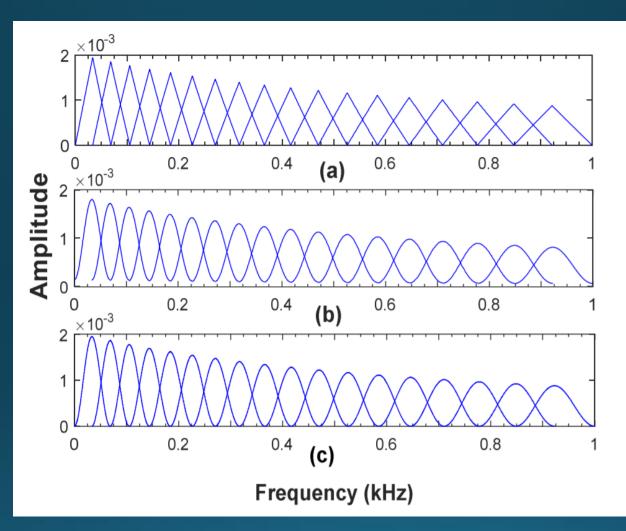
- The EEG signal partitioned into 30s frames
- Each frame is multiplied by a window function to form an epoc
- Discrete Fourier Transform (DFT) of epocs are calculated
- Absolute value DFT is fed to a set of frequency scaled filters (filterbank)
- Each filter output is summed over frequency
- Their log values forms energy quantities of the filter bands
- Discrete Cosine Transform (DCT) of the logarithm spectrum values is calculated to switch back to the time domain
- This gives the cepstrum coefficients to form the feature vector

Feature Extraction Diagram



Filterbank

- Filterbank filters are constructed using three different windowing functions
 - Triangular
 - Hamming
 - Hanning
- Three frequency warping functions are also utilized
 - Linear
 - Mel
 - Bark



Magnitude normalized and linear warping scaled filterbank filters in kHz region

Classification

- Sleep classification is performed with well-known supervised machine learning algorithm SVM
 - Training: SVM binary classifier learns a separating hyperplane between two classes to maximize the margin (distance) between the closest training samples (support vectors) and that hyperplane based on the training data
 - Test: SVM decides the class of each test data point by determining its position relative to that hyperplane
- SVM model can be mapped to a transform space (a higher dimensional space) through the use of a non-linear mapping (kernel function)
- Multiple classification in SVM
 - first converted to binary classification problems, then solved
 - commonly used methods: one-against-one and one-against-all

Database

Single (Pz-Oz) channel EEG of Sleep-EDF database is used in this study(*)

- Obtained in a hospital from eight Caucasian males and females, aged between 21-35, not on medication
- Four of the signals from healthy volunteers, recorded for over 24 hours
- Other four, healthy subjects with slight sleep disorder, collected during night time
- Sampling frequency: 100 Hz
- Sleep stages are scored for 30 second epocs according to R & K standards

(*): https://physionet.org/physiobank/database/sleep-edf/

Performance Measure

Sensitivity (SN), Specificity (SP) and percent Correct Classification Ratio (CCR) are utilized as the performance measure of the test of any epoc being in a particular class

$$SN = \left(\frac{TP}{TP + FN}\right) \times 100$$
$$SP = \left(\frac{TN}{TN + FN}\right) \times 100$$
$$CCR = \left(\frac{TP + TN}{TP + FN + FP + TN}\right) \times 100$$

All defined in terms of

- True Positive (TP)
- False Negative (FN)
- False Positive (FP)
- True Negative (TN)

test results

Performance Measure

- True Positive (TP): an epoc (labeled in that particular class in database) correctly classified
- False Negative (FN): an epoc (labeled in that particular class in database) incorrectly classified to a different class
- False Positive (FP): an epoc (not labeled in that particular class in database) is incorrectly classified to that class
- True Negative (TN): an epoc (not labeled in that particular class in database) is correctly classified

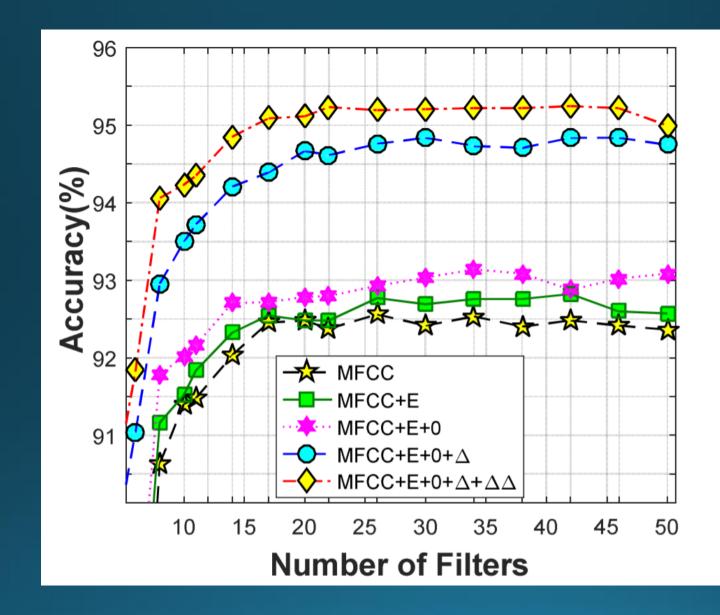
Selection of Training and Test Data

- Validation Set (*) is used to compare the study results with the available published results
- Half of the data is used as the training set
- Other half is used as test set
- Repeated for ten times
- All results are averaged

(*): A.R. Hassan and M.I.H. Bhuiyan, "Computer-aided sleep staging using complete ensemble empirical mode decomposition with adaptive noise and bootstrap aggregating", Biom. Signal Process Control 24, pp. 1–10, 2016

Results

- Filter set parameters giving the highest CCR ratio is investigated
- Linear, Mel and Bark scales are used for the triangular filter (common filterbank type used in most of the studies in the literature)
- Also included test result obtained with the use of expanded features
 - energy of epoc (E)
 - zero order coefficient (o)
 - cepstrum coefficients first order derivatives (Δ)
 - cepstrum coefficients second order derivatives ($\Delta\Delta$)
- Each new term included in the feature vector increased the test performance



Results

- Highest CCR result is obtained for the number of filters is about 32 (linear scaling) and 43 (Mel scaling)
- No significant difference between the performances of the scaling types
- The best CCR results obtained in this work for LFCC + o + E + Δ + $\Delta\Delta$ and MFCC + o + E + Δ + $\Delta\Delta$ are 95.39 and 95.28, respectively
- Confusion matrix with Sensitivity, Specificity and CCR results are also presented

	AWAKE	NREM	REM	% SN	% SP
AWAKE	4000	20	8	99.30	96.45
NREM	96	2584	80	93.62	97.33
REM	24	108	674	83.62	98.68
% ACC	95.58				

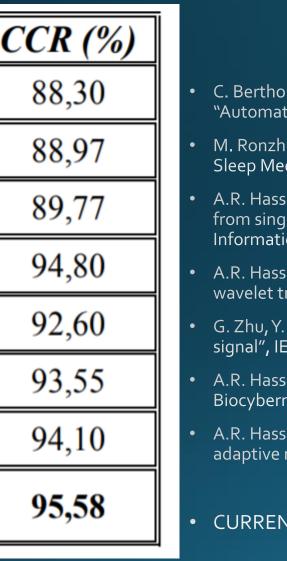
Confusion Matrix, Sensitivity, Specificity and CCR for LFCC + $o + E + \Delta + \Delta\Delta$ feature set

• Hamming and Hanning window based filterbank performance also studied

Type of filterbank	CCR (%)
$LFCC + 0 + E + \Delta + \Delta\Delta + Triangular$	95,39
$LFCC + 0 + E + \Delta + \Delta\Delta + Hamming$	95,52
$LFCC + 0 + E + \Delta + \Delta\Delta + Hanning$	95,40
$LFCC + 0 + E + \Delta + \Delta\Delta + Triangular + Normalize$	95,47
$LFCC + 0 + E + \Delta + \Delta\Delta + Hamming + Normalize$	95,58
$LFCC + 0 + E + \Delta + \Delta\Delta + Hanning + Normalize$	95,48

• LFCC + o + E + Δ + $\Delta\Delta$ feature set for 32 filters in the filterbank results

• The average percent CCR result 95.58



GlobalSIP 2017

Comparison

- C. Berthomier, X. Drouot, M. Herman-Stoca, P. Berthomier, J. Prado, D. BokarThire, O. Benoit, J. Mattout and M.-P. d'Ortho, "Automatic analysis of single-channel sleep EEG: validation in healthy individuals", Sleep 30 (11), pp. 1587–1595, 2007.
- M. Ronzhina, O. Janošuek, J. Kolárová, M. Nováková, P. Honzík, and I. Provazník, "Sleep scoring using artificial neural networks", Sleep Med. Rev. 16 (3), pp. 251–263, 2012.
- A.R. Hassan, S.K. Bashar and M.I.H. Bhuiyan, "On the classification of sleep states by means of statistical and spectral features from single channel electroencephalogram", International Conference on Advances in Computing, Communications and Informatics (ICACCI), pp. 2238-43, 2015.
- A.R. Hassan and M.I.H. Bhuiyan, "A decision support system for automatic sleep staging from EEG signals using tunable g-factor wavelet transform and spectral features", J. Neurosci. Methods 271, pp. 107–118, 2016.
- G. Zhu, Y. Li and P. Wen, "Analysis and classification of sleep stages based on difference visibility graphs from a single channel EEG signal", IEEE J Biomed Health Inform, pp. 99-1, 2014
- A.R. Hassan and M.I.H. Bhuiyan, "Automatic sleep scoring using statistical features in the EMD domain and ensemble methods", Biocybern. Biomed. Eng. 36 (1), p 248–255, 2016.
- A.R. Hassan and M.I.H. Bhuiyan, "Computer-aided sleep staging using complete ensemble empirical mode decomposition with adaptive noise and bootstrap aggregating", Biom. Signal Process Control 24, pp. 1–10, 2016.
- CURRENT STUDY

21

Thanks for listening