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Introduction

Background

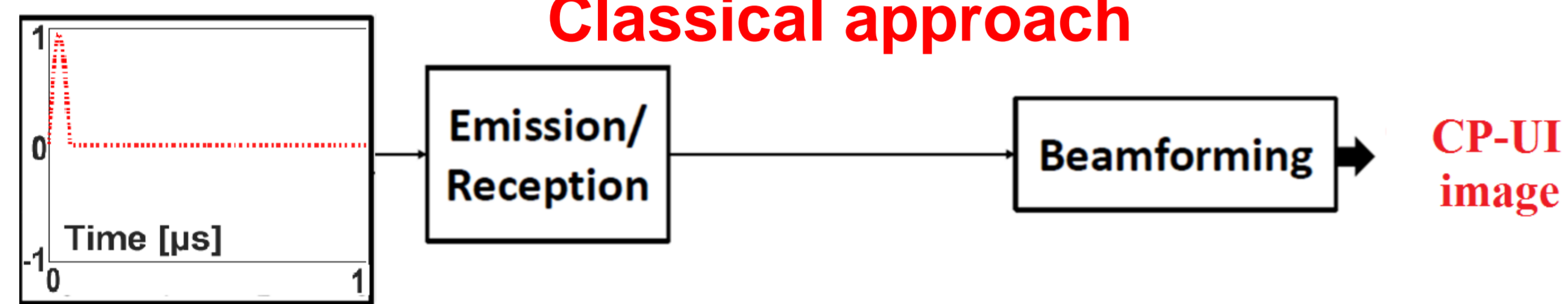
- Pulse compression technique called Resolution Enhancement Compression (REC) to increase the eSNR and the bandwidth of the received signals [1]
- Ultrafast Imaging (UI) through plane wave coherent compounding [2]

Objective of this study

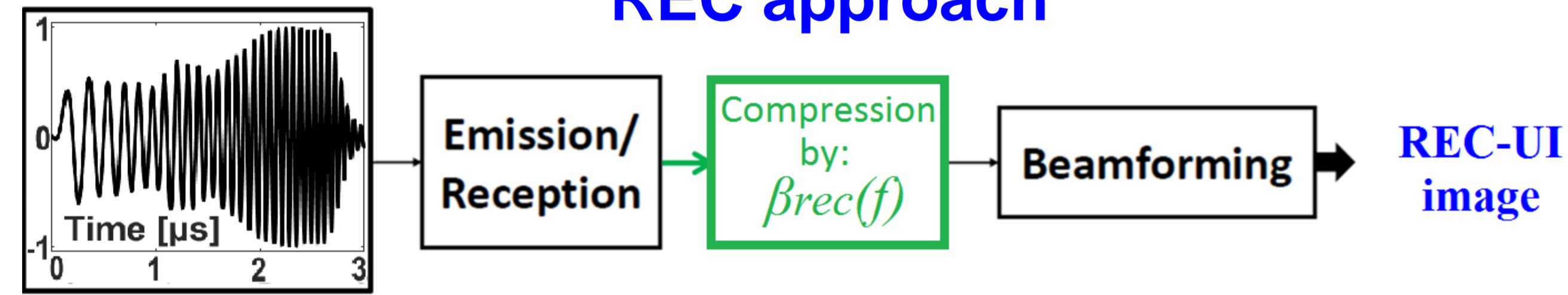
Experimental implementation on a research ultrasound scanner (UlaOp [3]) of a new method that combines UI with REC adapted to the attenuation effect of the imaged medium.

Methods

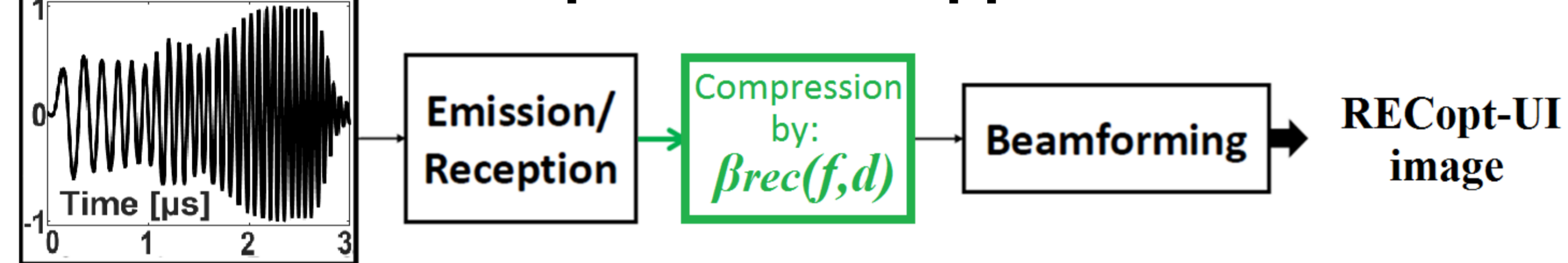
Classical approach



REC approach



Proposed REC approach



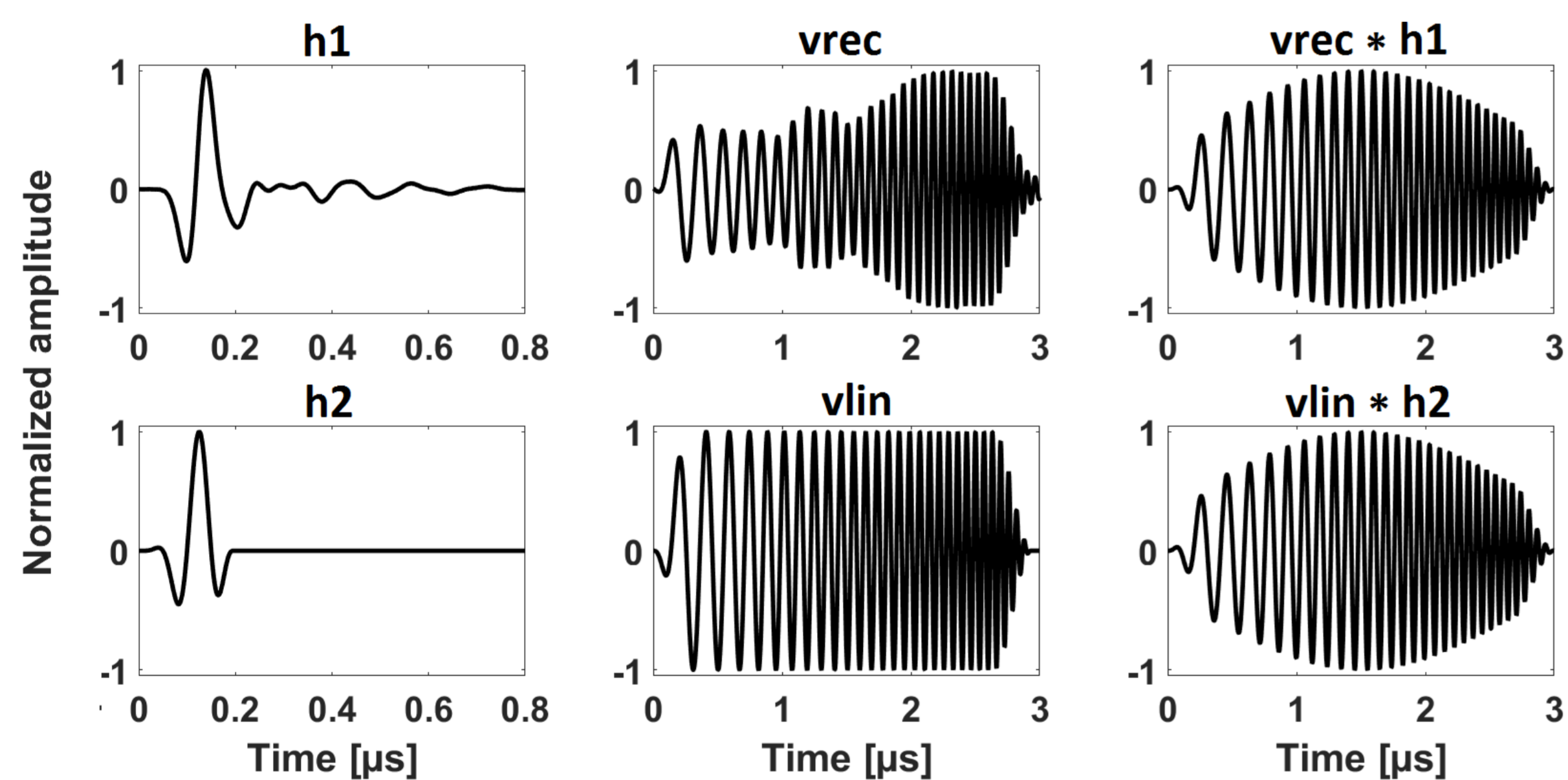
REC excitation signal $v_{rec}(t)$ comes from the equivalence between the real transducer and a fictive transducer with a higher bandwidth:

$$v_{rec}(t) * h_1(t) = v_{lin}(t) * h_2(t) \quad (1)$$

- ✓ $h_1(t)$: real impulse response (measured from a surface planar)
- ✓ $h_2(t)$: designed impulse response (broader than $h_1(t)$)
- ✓ $v_{lin}(t)$: linear chirp (weighted with a Tukey window)

- How to calculate $v_{rec}(t)$? \Rightarrow (1) in Fourier domain

$$V_{REC}(f) = V_{REC}(f) \frac{H_2(f)}{H_1(f)} \rightarrow V_{REC}(f) = V_{REC}(f) \frac{H_2(f)H_1^*(f)}{|H_1(f)|^2 + |H_1(f)|^{-2}}$$



REC compression:

$$\beta_{REC}(f) = \frac{V'_{LIN}(f)}{|V'_{LIN}(f)|^2 + \gamma e^{SNR^{-1}}(f)} \quad \text{with: } V'_{LIN}(f) = V_{REC}(f) \frac{H_1(f)}{H_2(f)}$$

RECopt compression

$$H_{att}(f, d) = e^{-ad|f|} \times e^{-j2\pi f \tau d} \times e^{-j \frac{2f a d}{\pi} \ln(2\pi f)} \quad \text{with: } \tau = \tau_b + \frac{\alpha}{\pi^2} \tau_m$$

$\tau_b = 6.67 \mu s/cm$, is the bulk delay; $\tau_m = 20$, is the minimum-phase delay factor; α is the attenuation of the imaged medium, d is the distance between the probe and the considered depth [4].

$$\beta_{RECopt}(f, d) = \frac{V'_{LIN}(f, d)}{|V'_{LIN}(f, d)|^2 + \gamma e^{SNR^{-1}}(f)}$$

$$\text{with: } V'_{LIN}(f) = V_{REC}(f) \frac{H_1(f)H_{att}(f, d)}{H_2(f)}$$

- ✓ $\gamma e^{SNR^{-1}}$: can be tuned in order to adjust the tradeoff between axial resolution and eSNR

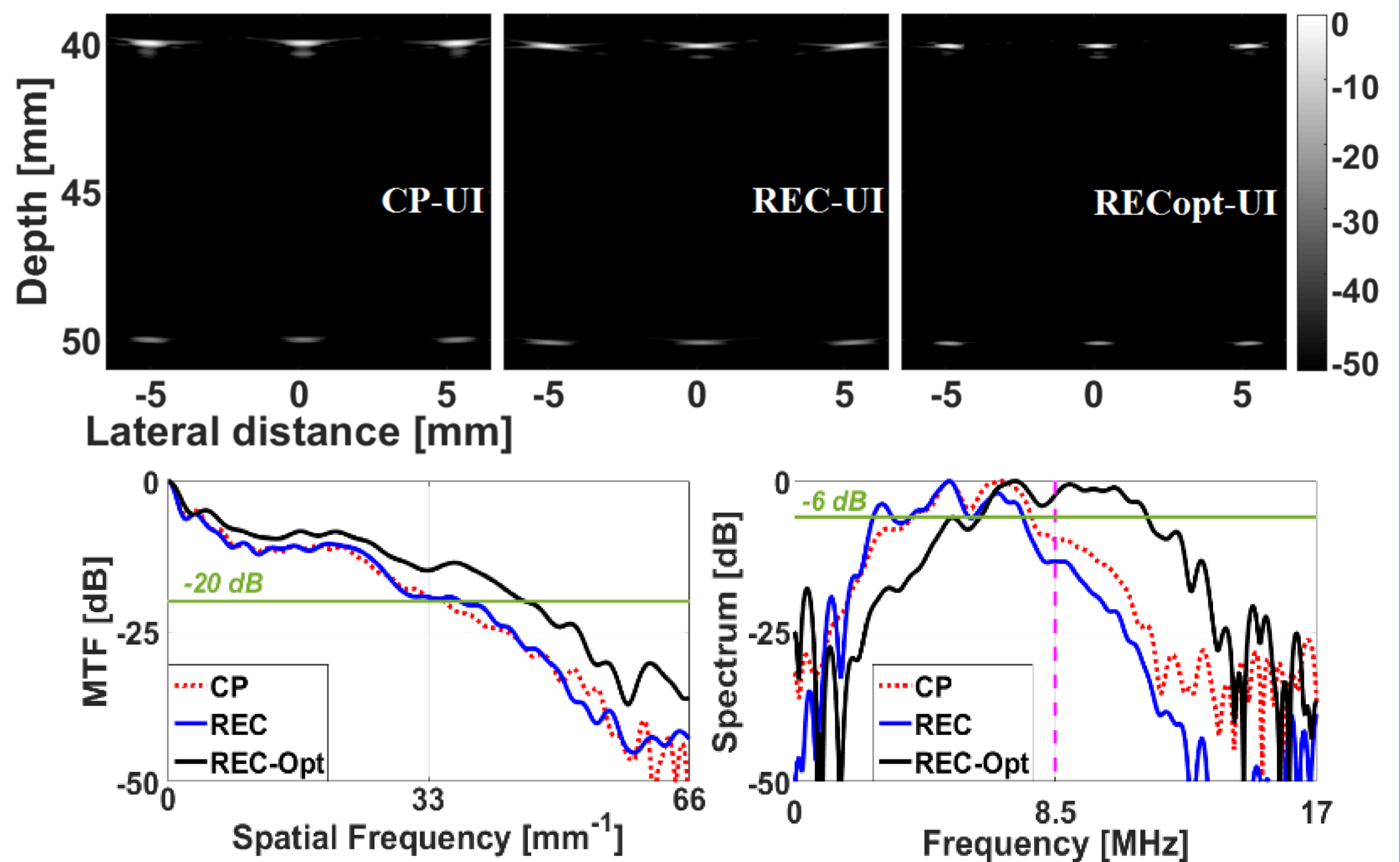
Acquisition parameters

UlaOp having 64 channels data, equipped with a linear array model LA 523E

- ✓ Pitch = 245 μm , $f_0 = 8.5$ MHz, $f_s = 50$ MHz
- ✓ 27 plane waves in transmission separated by 0.67° between -9° and $+9^\circ$

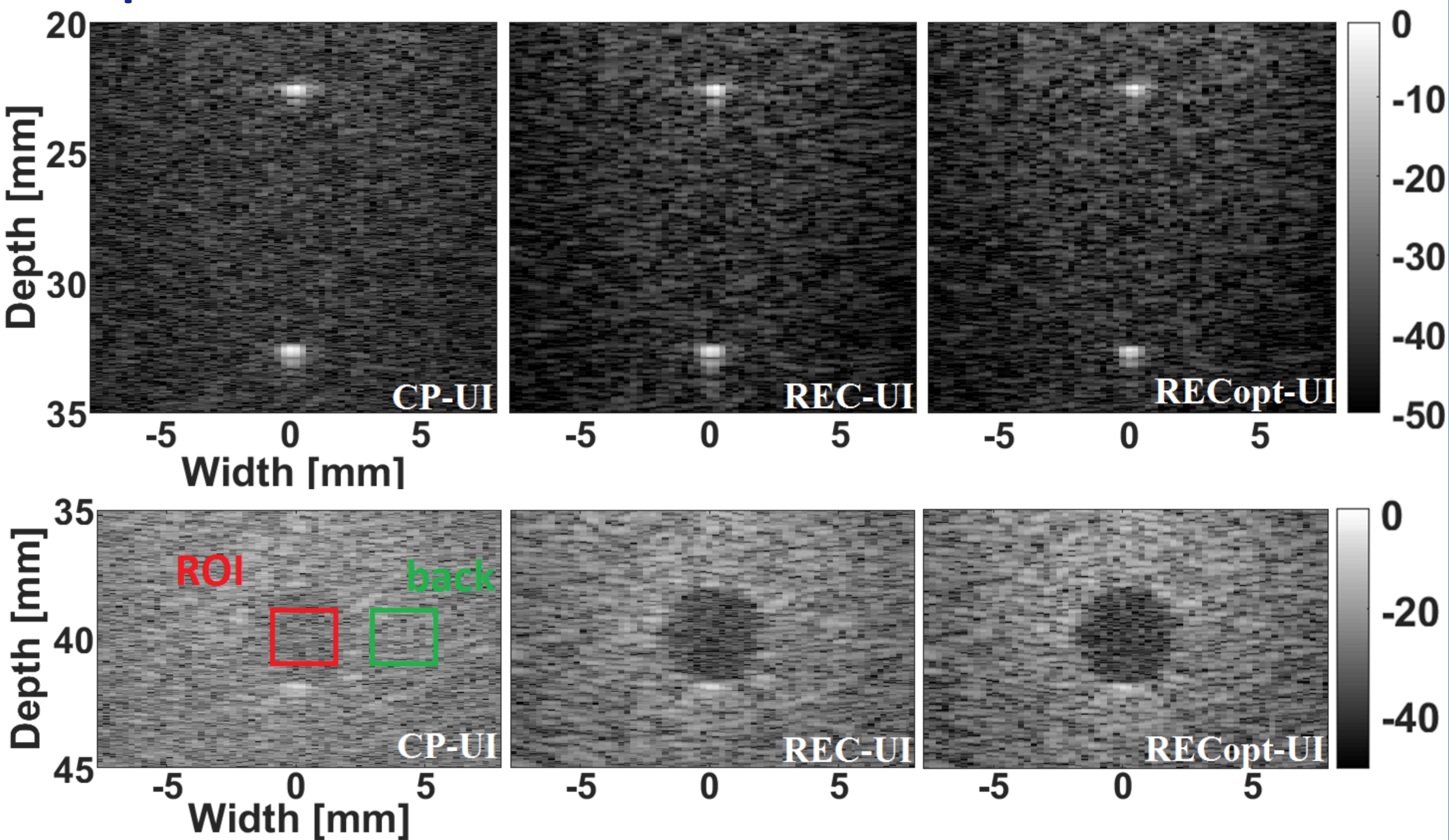
Results

Simulation results



Metrics	CP-UI	REC-UI	RECopt-UI	Enhancements	
				RECopt-UI vs CP-UI	RECopt-UI vs REC-UI
MTF (mm^{-1})	35.5	37.1	47.2	+ 33.0 %	+ 27.2 %
Bandwidth (MHz)	3.85	4.04	5.45	+ 29.4 %	+ 25.9 %
eSNR (dB)	19.9	27.7	30.1	+10.2 dB	+2.4 dB

Experimental results



Metrics	CP-UI	REC-UI	RECopt-UI	Enhancements	
				RECopt-UI vs CP-UI	RECopt-UI vs REC-UI
Axial resolution (μm)	218.2	211.6	167.9	+ 30.0 %	+ 26.0 %
Bandwidth (MHz)	2.54	2.61	3.57	+ 28.9 %	+ 26.9 %
SNR (dB)	14.8	16.1	18.2	+ 3.4 dB	+ 2.1 dB
CNR (dB)	-4.31	4.32	5.49	+ 9.8 dB	+ 1.2 dB

Conclusion

- The experimental results show that REC adapted to the medium attenuation provides a better image quality than classical REC and than CP.
- This study proves that, by adapting the impulse response and the attenuation coefficient, this method can be implemented on a research scanner using any ultrasound probe.

- [1] M. L. Oelze, "Bandwidth and resolution enhancement through pulse compression," IEEE TUFFC, 2007.
 [2] G. Montaldo, M. Tanter, J. Bercoff, N. Benech, and M. Fink "Coherent Plane-Wave Compounding for Very High Frame Rate Ultrasonography and Transient Elastography," IEEE TUFFC, 2009.
 [3] P. Tortoli, L. Bassi, E. Boni, A. Dallai, F. Guidi, and S. Ricci, "UlaOp: an advanced open platform for ultrasound research," IEEE TUFFC, 2009.
 [4] K. V. Gurumurthy, and R. Martin Arthur "A dispersive model for the propagation of ultrasound in soft tissue," Ultrasonic Imaging, 1982.