

Joint Estimation of Activity Signal and HRF in fMRI using Fused LASSO

Priya Aggarwal¹, Anubha Gupta¹, and Ajay Garg²

¹SBILab, Department of Electronics and Communication Engineering (ECE),
IIT-Delhi, India

²Department of Neuroradiology, Neurosciences Centre, AIIMS, Delhi, India

Dec. 15, 2015
GLOBALSIP 2015



INDRAPRASTHA INSTITUTE of
INFORMATION TECHNOLOGY
DELHI

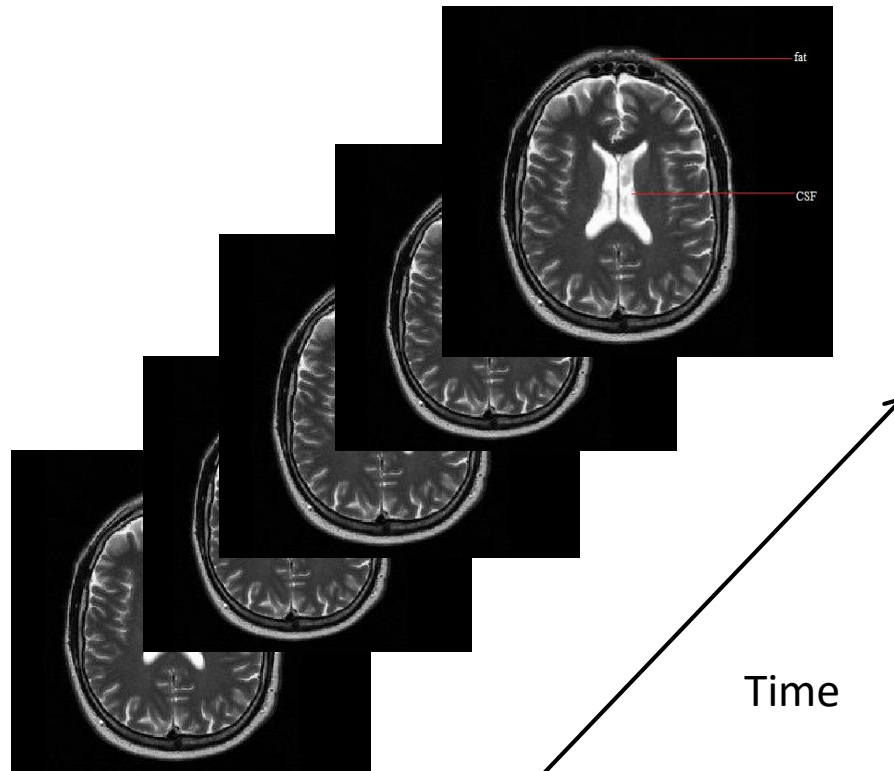
Presented by: Anubha Gupta

Outline of the Presentation



- Motivation
- Proposed work on joint estimation of HRF and activity signal
- Validation of the proposed method
 - on synthetic data
 - on real fMRI data
- Conclusion

Functional Brain Imaging (fMRI)



fMRI signal processing

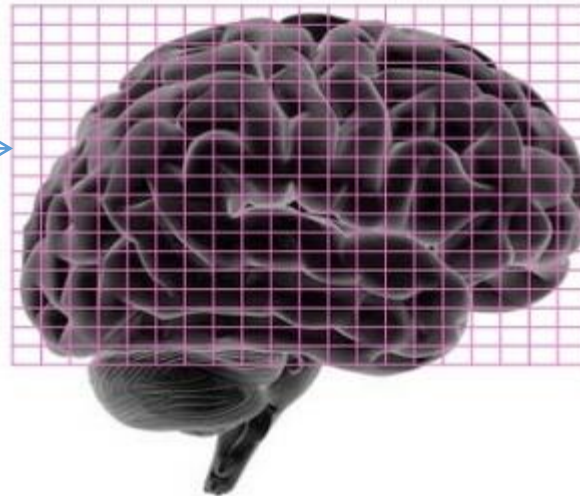


Input stimulus to perform
cognitive task

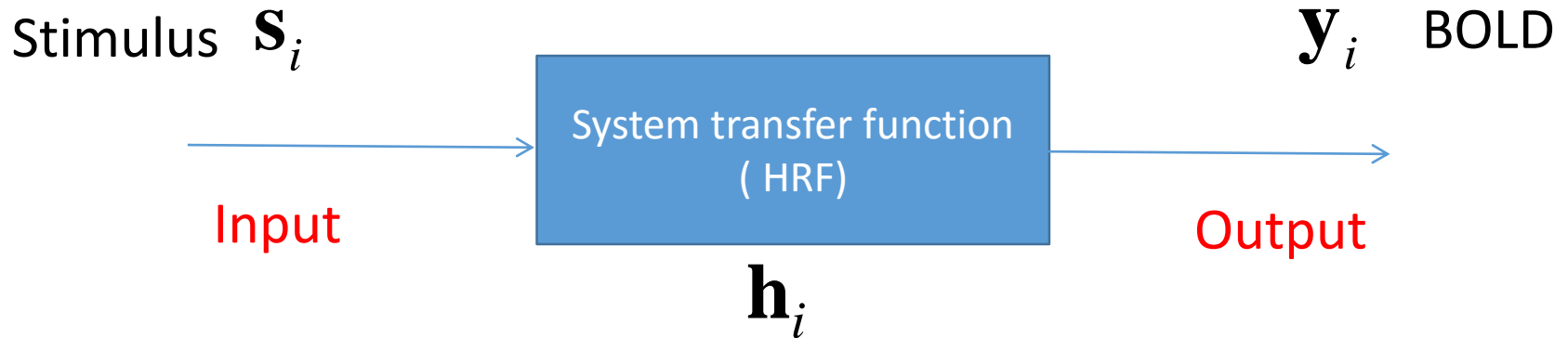
Detect brain activity

Input

Output



Motivation



fMRI voxel time series

$$\mathbf{y}_i = \mathbf{s}_i \otimes \mathbf{h}_i + \xi_i \quad \dots(1)$$

fixed canonical HRF

$$\mathbf{y}_i = \mathbf{s}_i \otimes \mathbf{h}_i + \xi_i \quad \text{.....(1)}$$

$$\mathbf{y}_i = \mathbf{S}\mathbf{h}\alpha_i + \xi_i \quad \text{-----(2)}$$

- Only unknown in equ.1 is intrinsic stimuli

HRF shape may vary across different brain regions as well as across patients.

Proposed Work



Aim: To propose a method for the joint estimation of HRF and activity signal

Proposed Joint Estimation Framework

1. Estimate underlying activity signal => via fused LASSO
2. Refine the HRF estimate

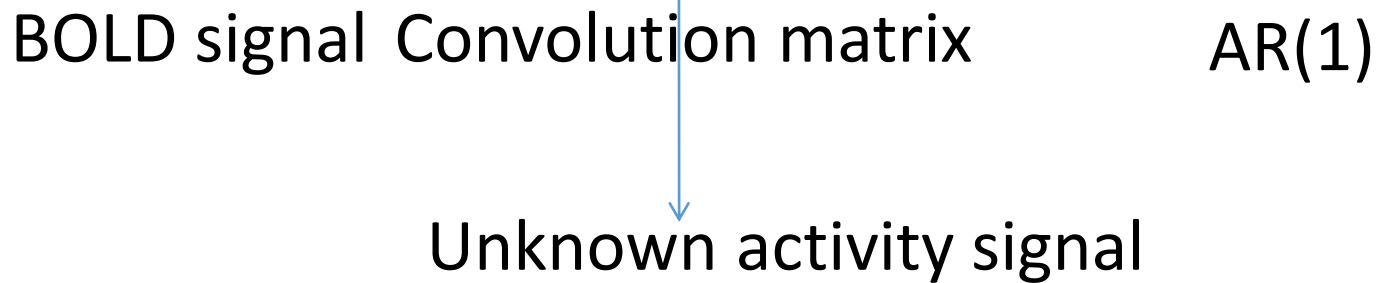
Iteratively

Step-1: Estimation of activity signal



$$\mathbf{y}_i = \mathbf{s}_i \otimes \mathbf{h}_i + \xi_i$$

$$\mathbf{y}_i = \mathbf{H} \mathbf{s}_i + \xi_i \quad \text{.....(3)}$$



Fused LASSO

$$\hat{\mathbf{s}}_i = \underset{\mathbf{s}_i}{\operatorname{argmin}} \left\| \mathbf{R}_v (\mathbf{y}_i - \mathbf{H}_i \mathbf{s}_i) \right\|_2 + \lambda_0 \|\mathbf{s}_i\|_1 + \lambda_1 \|\mathbf{T} \mathbf{s}_i\|_1$$

noise whitening matrix

noise covariance matrix $\mathbf{\Gamma}$ ($\mathbf{\Gamma}^{-1} = \mathbf{R}_v^T \mathbf{R}_v$)

.....(4)

$$\mathbf{\Gamma} = \frac{\sigma_v^2}{1 - \rho^2} \begin{bmatrix} 1 & \rho & \rho^2 & \dots & \rho^{n-1} \\ \rho & 1 & \rho & \dots & \rho^{n-2} \\ \cdot & \cdot & \cdot & \cdot & \cdot \\ \cdot & \cdot & \cdot & \cdot & \cdot \\ \rho^{n-1} & \dots & \rho^2 & \rho & 1 \end{bmatrix}$$

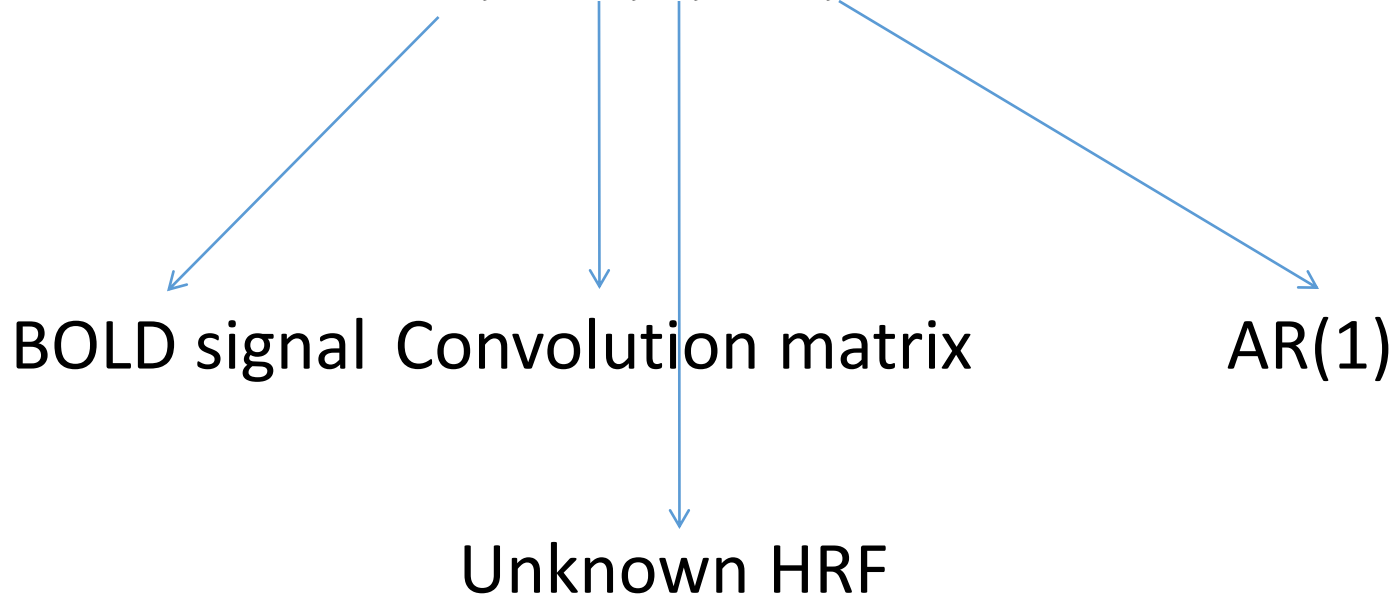
$$\mathbf{T} = \begin{bmatrix} -1 & 1 & 0 & \cdot & \cdot & 0 & 0 \\ 0 & -1 & 1 & 0 & \cdot & \cdot & 0 \\ 0 & 0 & -1 & 1 & 0 & \cdot & \cdot \\ 0 & 0 & \cdot & \cdot & \cdot & \cdot & \cdot \\ \cdot & \cdot & \cdot & \cdot & \cdot & \cdot & 0 \\ 0 & \cdot & \cdot & \cdot & 0 & -1 & 1 \\ 0 & 0 & \cdot & 0 & 0 & 0 & -1 \end{bmatrix}$$

Step-2: Estimation of HRF



$$\mathbf{y}_i = \mathbf{s}_i \otimes \mathbf{h}_i + \xi_i$$

$$\mathbf{y}_i = \mathbf{S}_i \mathbf{h}_i + \xi_i \quad \text{.....(5)}$$



Step-2: Estimation of HRF

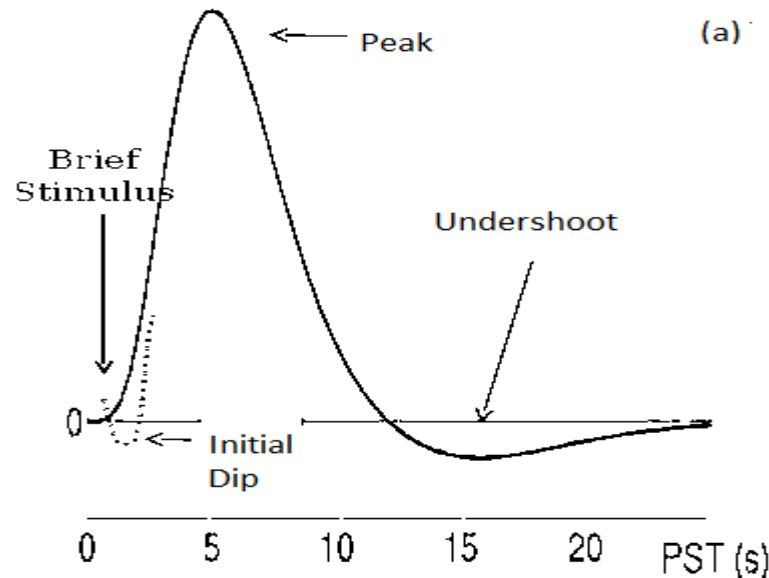
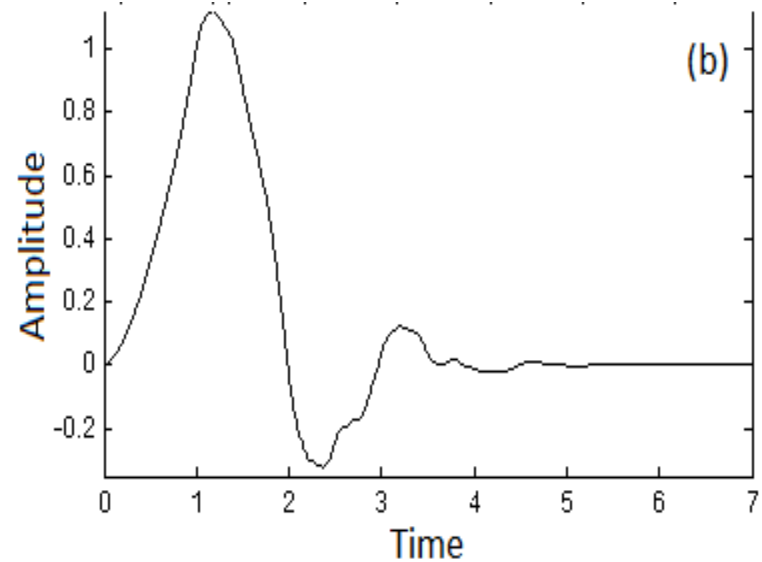


Fig. 1. (a): Theoretical shape of HRF;



(b) Scaling function of *db4*

Assumptions on HRF:

- 1) Smooth over time;
- 2) Sparse in wavelet domain (with db4)

$$\hat{\mathbf{h}}_i = \underset{h_i}{\operatorname{argmin}} \|\mathbf{R}_v(\mathbf{y}_i - \mathbf{S}_i \mathbf{h}_i)\|_2 + \lambda_2 \|\mathbf{D} \mathbf{h}_i\|_2 + \lambda_3 \|\mathbf{W} \mathbf{h}_i\|_1$$

$$\mathbf{D} = \begin{bmatrix} 2 & -1 & 0 & \cdot & \cdot & 0 & 0 \\ -1 & 2 & -1 & 0 & \cdot & \cdot & 0 \\ 0 & -1 & 2 & -1 & 0 & \cdot & \cdot \\ 0 & 0 & \cdot & \cdot & \cdot & \cdot & \cdot \\ \cdot & \cdot & \cdot & \cdot & 2 & -1 & 0 \\ 0 & \cdot & \cdot & \cdot & -1 & 2 & -1 \\ 0 & 0 & \cdot & 0 & 0 & -1 & 2 \end{bmatrix}$$

.....(6)

Matrix operator
for *db4*

Table-1**Pseudo Code for the Iterative Joint Estimation framework****Input Parameters**

Tikhonov regularisation matrix \mathbf{D} (size $L \times L$)

Fused LASSO matrix \mathbf{T} (size $M \times M$)

Daubechies-4 matrix \mathbf{W} (size $L \times L$)

Initialize HRF matrix \mathbf{H}_i (size $M \times M$)

Lagrangian multipliers λ_1 , λ_2 , and λ_3 (scalars)

Noise covariance matrix $\mathbf{\Gamma}$

Input Data

Measured voxel V_i 's time series stacked in a column r_i
(size $M \times 1$)

Start

Step-1 $\mathbf{y}_i = \text{detrend}(r_i)$

Step-2 Compute estimate of activity signal $\hat{\mathbf{s}}_i$

$$\hat{\mathbf{s}}_i = \arg \min_{\mathbf{s}_i} \|\mathbf{R}_v(\mathbf{y}_i - \mathbf{H}_i \mathbf{s}_i)\|_2 + \lambda_0 \|\mathbf{s}_i\|_1 + \lambda_1 \|\mathbf{T} \mathbf{s}_i\|_1$$

Step-3 Compute estimate of HRF $\hat{\mathbf{h}}_i$ using $\hat{\mathbf{s}}_i$

$$\hat{\mathbf{h}}_i = \arg \min_{\mathbf{h}_i} \|\mathbf{R}_v(\mathbf{y}_i - \mathbf{S}_i \mathbf{h}_i)\|_2 + \lambda_2 \|\mathbf{D} \mathbf{h}_i\|_2 + \lambda_3 \|\mathbf{W} \mathbf{h}_i\|_1$$

Repeat Step-2 and Step-3 until the shapes of $\hat{\mathbf{s}}_i$ and $\hat{\mathbf{h}}_i$ converge.

Output $\hat{\mathbf{h}}_i$ and $\hat{\mathbf{s}}_i$

Results on synthetic fMRI data



Synthetic HRF of length 32 is generated using the difference of two Gamma functions as below-

$$h[n] = \left(\frac{n}{a_1 b_1} \right)^{a_1} e^{-\frac{(n-a_1 b_1)}{b_1}} - c \left(\frac{n}{a_2 b_2} \right)^{a_2} e^{-\frac{(n-a_2 b_2)}{b_2}} \dots\dots(7)$$

with $a_1=6$, $a_2=12$, $b_1=b_2=6$, and $c=0.35$.

Synthetic stimulus of 200 time points is generated with 5 ON periods of duration 6s, 5s, 10s, 3s, and 1s with onsets at 10s, 40s, 100s, 140s, and 180s, respectively.

Results on synthetic fMRI data



- Black solid line shows the actual HRF used in simulation set-up
- Box plot shows estimated HRF over 500 realizations of noise time-series

$$\lambda_0=0.001, \lambda_1=0.3, \lambda_2=1, \lambda_3=0.7, \sigma^2=0.1$$

- Black solid line shows the actual stimulus used in simulation set-up
- Box plot shows estimated stimulus over 500 realizations of noise time-series

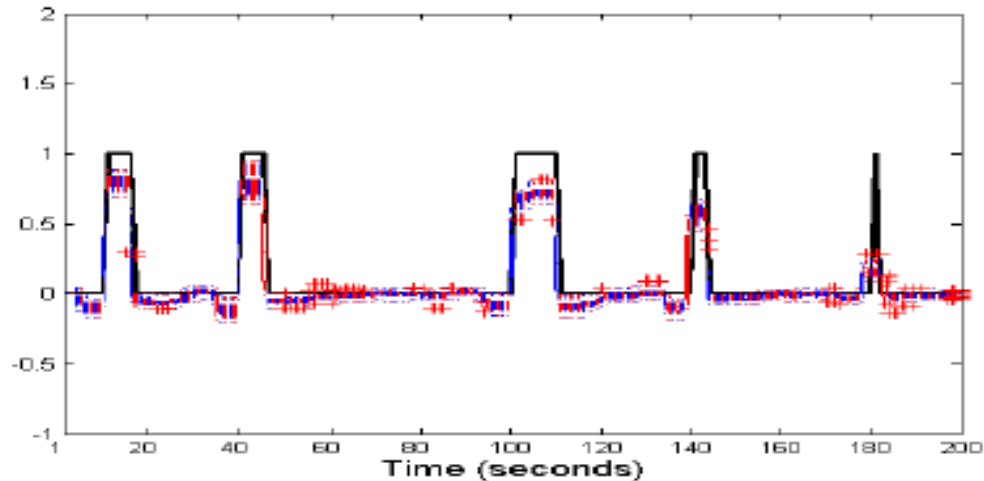
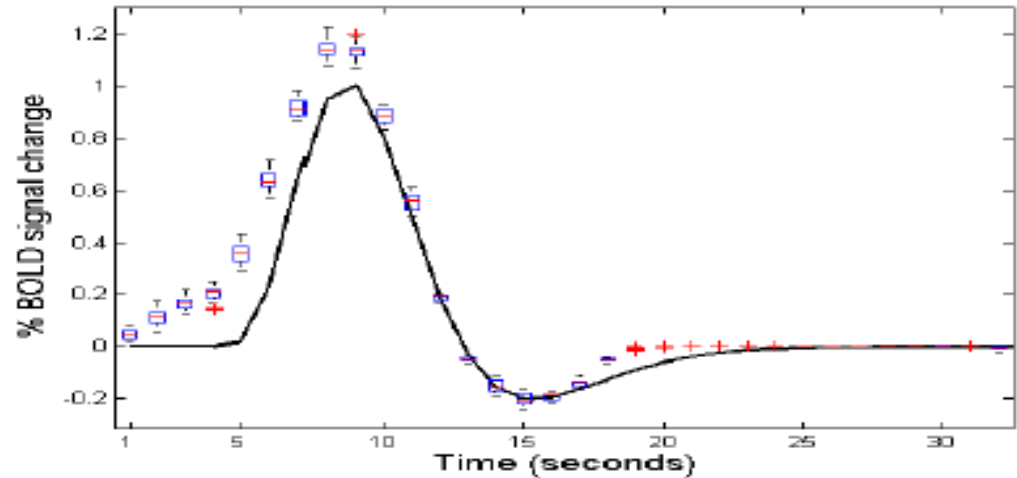


Fig. 2: (a): Estimated HRF; (b) Estimated Activity Signal

Table-2: MSE calculated between estimated and the actual HRF (that is used in the synthetic data)

	<i>Noise Variance σ^2</i>				
	0.05	0.1	0.25	0.5	0.75
MSE using the Proposed method	0.0151	0.0159	0.0171	0.0183	0.0220

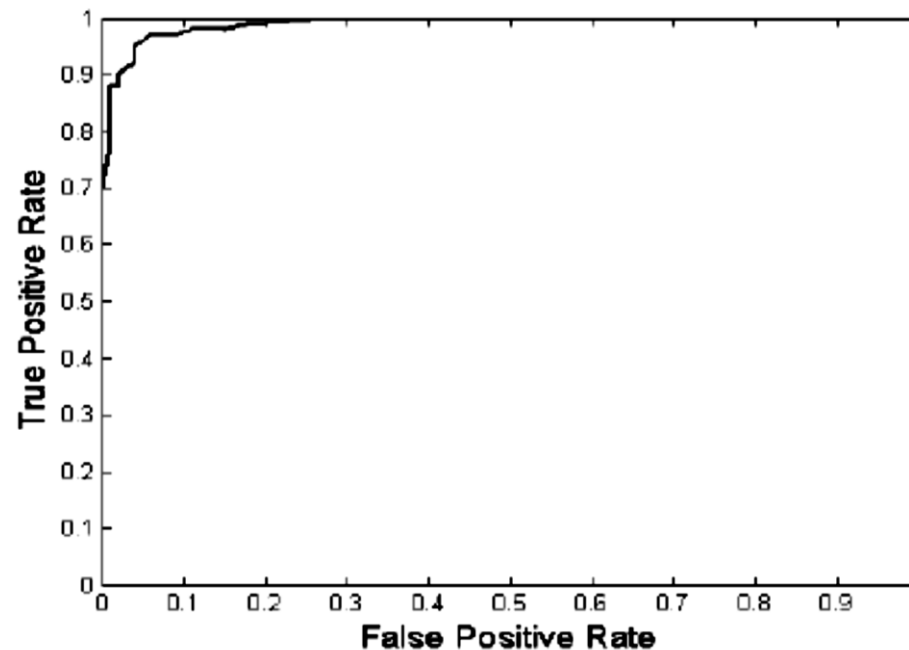


Fig.3: ROC curve on the estimated activity signal for single voxel time series with $\sigma^2=0.25$.

Results on real fMRI data



Real fMRI data --- a right hand finger tapping task in 3-T MR scanner

- 36 contiguous slices with 128x128x36 voxels, voxel size = 4x4x4 mm³
- No. of brain volumes= 100, TR= 3s
- Stimulus: 10 volumes of rest followed by 10 volumes of activity, and so on
- Preprocessing: Using SPM12 -- include realignment (with the first scan for removal of motion artefact), slice time correction (with the first slice of each volume), and normalization (with the MNI atlas)
- Resultant fMRI data had 100 brain volumes of 79x95x68 voxels each
- No smoothing is done in preprocessing
- First 12 dummy scans were discarded resulting in 88 brain volumes

Results on real fMRI data

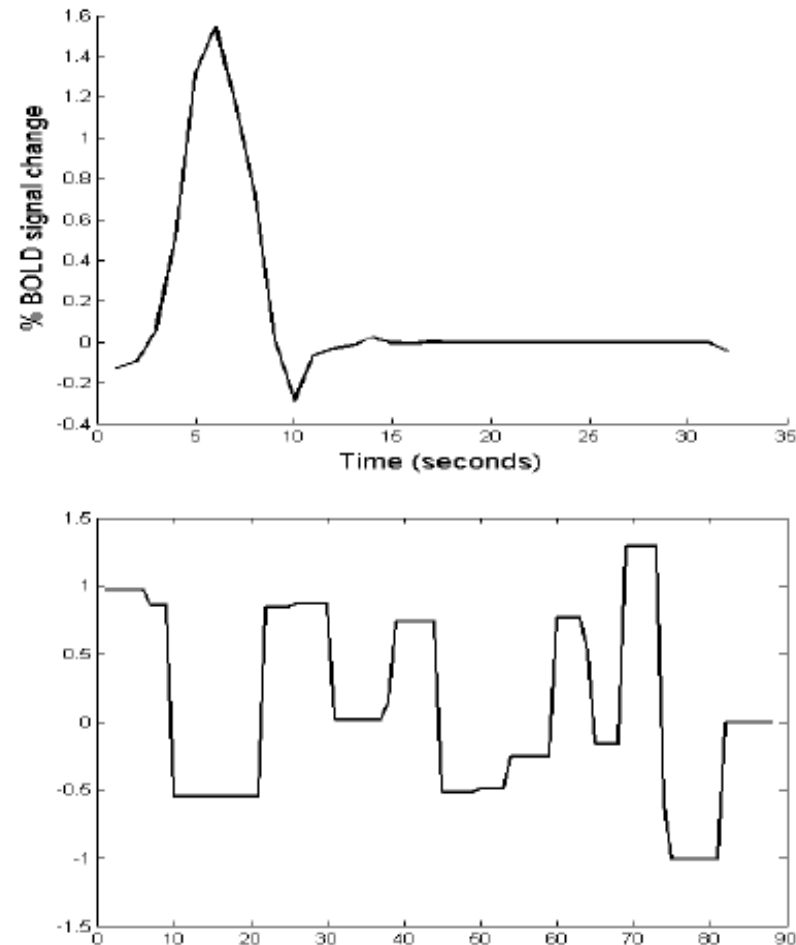


Fig. 5: (a): Estimated HRF; (b) Estimated Activity Signal at voxel (40, 43, 66) using the proposed method

Results on real fMRI data (Highest norm voxel)

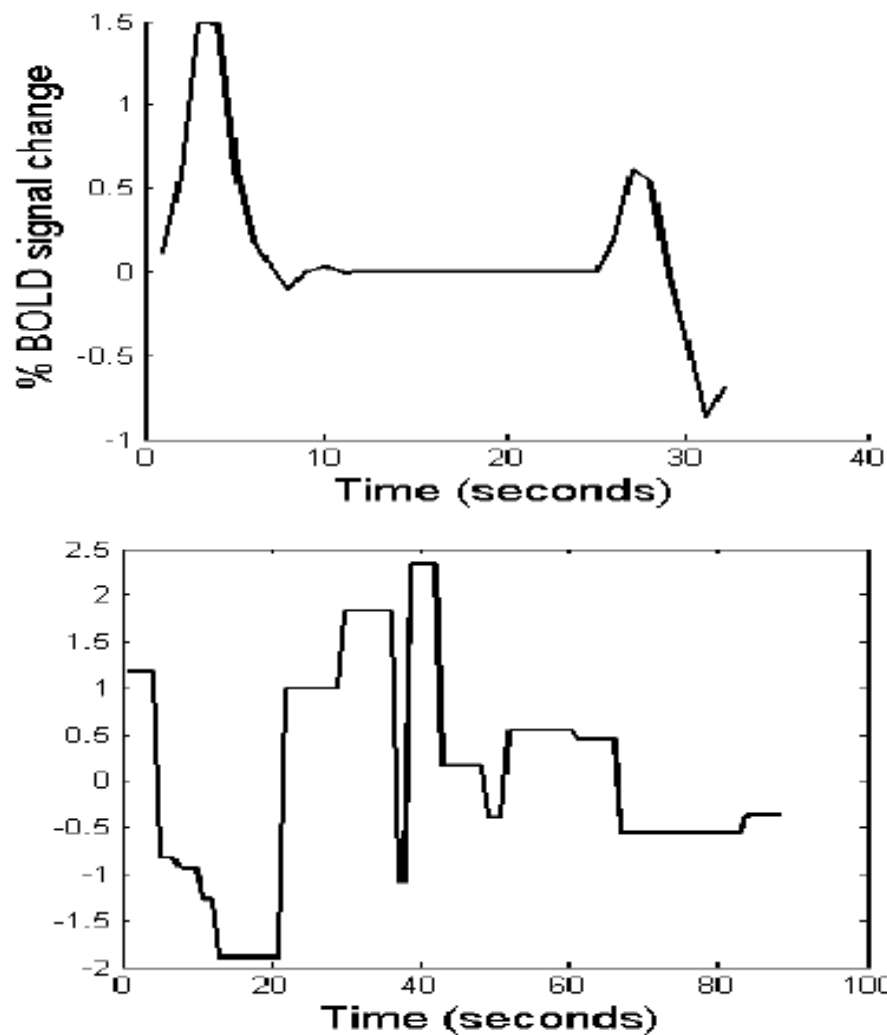


Fig. 6: (a): Estimated HRF; (b) Estimated Activity Signal at voxel (41, 45, 66) using the proposed method

- Joint iterative framework for the estimation of HRF and the underlying activity signal
- Two stage optimization that estimates activity signal and HRF iteratively
- Can be applied to both task-based and the Resting-state data
- The proposed method is observed to perform satisfactorily

References



- G. Glover, “Deconvolution of impulse response in event related BOLD fMRI,” *Neuroimage*, vol. 9, pp. 416-429, 1999.
- F. I. Karahanolu, et al., “Total activation: fmri deconvolution through spatio-temporal regularization,” *Neuroimage*, vol. 73, pp. 121–134, 2013.
- Z. Dogan, T. Blu and D. V. D. Ville, “Detecting spontaneous brain activity in functional Magnetic Resonance Imaging under finite rate of innovation,” *IEEE ISBI*, pp. 1047–1050, April 2014.
- C. C. Gaudes, et al., “Paradigm free mapping with sparse regression automatically detects single-trial functional magnetic resonance imaging blood oxygenation level dependent responses,” *Human Brain Mapping*, vol. 34, no. 3, pp. 501–518, 2013.
- C. C. Gaudes, et al., “Structured sparse deconvolution for paradigm free mapping of functional MRI data,” *IEEE ISBI*, vol. 34, no. 3, pp. 322–325, May 2012.
- I. Khalidov, et al., “Activelets and sparsity: A new way to detect brain activation from fMRI data,” *Signal Processing*, pp. 2810–2811, 2011.
- R. Tibshirani, et al., “Sparsity and smoothness via the fused lasso,” *Journal Of The Royal Statistical Society Series*, vol. 67, pp. 91–108, 2005.
- F. Ahmad, et al., “Regularization of voxelwise autoregressive model for analysis of functional magnetic resonance imaging data,” *Wiley Magnetic Resonance*, vol. 38, pp. 187–196, 2011.

- P. Aggarwal, A. Gupta, and A. Garg, "Joint Estimation of Hemodynamic Response Function and Voxel Activation in functional MRI Data," Accepted, MICCAI, October 2015.
- Bezargani and A. Nostratinia, "Joint maximum likelihood estimation of activation and Hemodynamic Response Function for fMRI," *Elsevier Medical Image Analysis*, vol. 18, pp. 711-724, 2014.
- <http://www.lion.ucl.ac.uk/spm/data/>
- Maldjian, J. A. Laurienti et al., "An automated method for neuroanatomic and cytoarchitectonic atlas-based interrogation of fmri data sets (WFU Pickatlas, version 3.05)," *NeuroImage*, vol. 19, pp. 1233-1239.
- M. Grant and S. Boyd, "CVX: Matlab software for disciplined convex programming, version 2.0 beta. <http://cvxr.com/cvx>," September 2013.

Acknowledgement



The first author would like to thank Visvesvaraya research fellowship, Department of Electronics and Information Tech., Ministry of Communication and IT, Govt. of India, for providing financial support for this work.

Thank you