

Waveform Modeling by Adaptive Weighted Hermite Functions

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Outline

- 1 Introduction
- 2 Nonlinear model using Hermite functions
- 3 Case study: ECG compression

Motivation

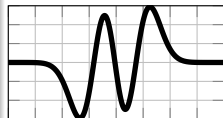
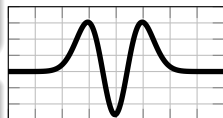
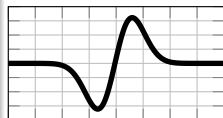
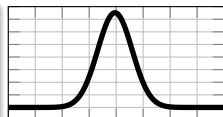
ECG signal modeling

Due to shape similarities, Hermite functions became very popular in

- modeling QRS shape features,
- ECG data compression,
- clustering QRS complexes,
- detecting abnormalities such as myocardial infarction,
- ECG segmentation and delineation.

Other applications

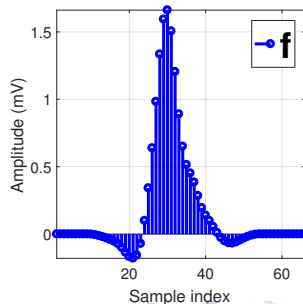
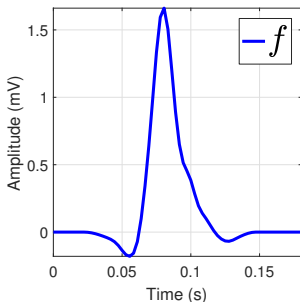
- Ballistocardiogram and myoelectric signal processing,
- image processing,
- computer tomography,
- radar signal processing, and
- physical optics.



Signal representation

Notations

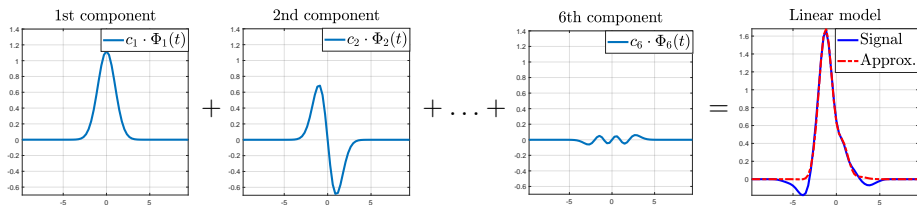
- Continuous signal: $f : \mathbb{R} \rightarrow \mathbb{R}$.
- Sampling period: T .
- Discrete time instances: $t_i := i \cdot T$.
- Discrete signal having n samples: $[\mathbf{f}]_i := f(t_i)$ for $i = 1, \dots, n$.



Linear model

$$[\mathbf{f}]_i = f(t_i) \approx \sum_{k=1}^m c_k \Phi_k(t_i) = (\Phi \mathbf{c})_i \quad (i = 1, \dots, n)$$

- $\{\Phi_k \mid 1 \leq k \leq m\}$ can be the set of trigonometric or Walsh functions, wavelets, orthogonal polynomials, splines, etc.
- The least squares (LS) estimate of the coefficients is $\mathbf{c} = \Phi^+ \mathbf{f}$, where Φ^+ denotes the Moore–Penrose inverse of Φ .



Linear LS approximation of a QRS complex using Hermite functions (no optimization).

Nonlinear model

$$[\mathbf{f}]_i = f(t_i) \approx \sum_{k=1}^m c_k \Phi_k(t_i; \boldsymbol{\theta}) = (\boldsymbol{\Phi}(\boldsymbol{\theta})\mathbf{c})_i \quad (i = 1, \dots, n)$$

- The functions $\{\Phi_k(\cdot; \boldsymbol{\theta}) \mid 1 \leq k \leq m\}$ are parametrized by $\boldsymbol{\theta}$.
- \mathbf{c} and $\boldsymbol{\theta}$ are determined via nonlinear optimization.

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Nonlinear LS approximation of a QRS complex using Hermite functions parametrized by the dilation and the translation.

Nonlinear model

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Nonlinear LS approximation of a QRS complex using Hermite functions parametrized by the dilation and the translation (final optimization step).

Signal model

Goals

- Generalization of former wave shape models via weight modification.
- Adapt the new weighted Hermite system to various types of signals.
- Heuristics for speeding up the nonlinear optimization.
- Case study: electrocardiogram (ECG) signal compression.

Related works

- ECG data compression¹
- ECG segmentation²

¹T. Dózsa and P. Kovács, *ECG signal compression using adaptive Hermite functions*, *Advances in Intelligent Systems and Computing*, vol. 399, pp. 245–254, 2015.

²P. Kovács, C. Böck, J. Meier, M. Huemer, *ECG segmentation using adaptive Hermite functions*, *Proceedings of the 51st Asilomar Conference on Signals, Systems, and Computers*, 2017, pp. 1476–1480.

Hermite polynomials

Terminology

- Three-term recurrence relation:

$$h_{k+1}(t) = (t - \alpha_k) h_k(t) - \beta_k h_{k-1}(t), \quad (k \in \mathbb{N}).$$
$$h_{-1}(t) = 0, \quad h_0(t) = 1.$$

- Recurrence coefficients for monic Hermite polynomials:

$$\alpha_k = 0, \quad \beta_0 = \sqrt{\pi}, \quad \beta_k = k/2, \quad (k \in \mathbb{N}^+).$$

- Orthogonality:

$$\|h_k\|_2^2 \cdot \delta_{kj} = \langle h_k, h_j \rangle_w := \int_{-\infty}^{\infty} h_k(t) h_j(t) w(t) dt,$$

where $w(t) = e^{-t^2}$ is the Hermite weight function.

Hermite functions

Definition

- System of Hermite polynomials: $\{h_k \mid k \in \mathbb{N}\}$.
- System of Hermite functions: $\{\Phi_k \mid k \in \mathbb{N}\}$, where

$$\Phi_k(t) = h_k(t) / \|h_k\|_2 \cdot \sqrt{w(t)} \quad (k \in \mathbb{N}).$$

Affine argument transform

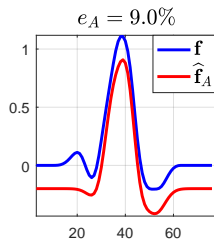
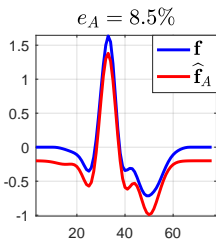
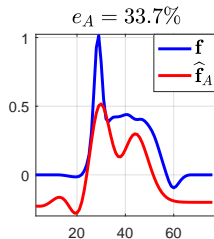
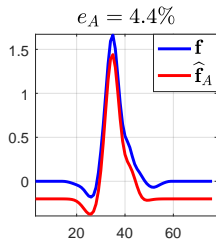
$$\Phi_k(t; \tau; \lambda) := \sqrt{\lambda} \Phi_k(\lambda(t - \tau)) \quad (t, \tau \in \mathbb{R}, \lambda > 0).$$

Optimization problem

Find λ, τ that minimize the so-called variable projection functional

$$r_2(\lambda; \tau) = \|\mathbf{f} - \Phi(\lambda; \tau) \Phi^+(\lambda; \tau) \mathbf{f}\|_2^2 = \|\mathbf{f} - \mathbf{P}_{\Phi(\lambda; \tau)} \mathbf{f}\|_2^2.$$

Hermite functions



Examples using 6 basis functions for which the affine Hermite model (red line) does not work perfectly.

Weighted Hermite functions

Modifying the weight function

- Let us define the class of weight functions:

$$\mathcal{V} = \{v(\cdot; \boldsymbol{\eta}) \in C(\mathbb{R}) : v \geq 0, \exists \gamma > 0, \sup_{t \in \mathbb{R}} |v(t; \boldsymbol{\eta})| e^{\gamma t^2} < \infty\}.$$

- $\{q_k \mid k \in \mathbb{N}\}$ is the set of orthogonal polynomials defined by $v \in \mathcal{V}$.
- Then the weighted Hermite functions are defined as follows:

$$\Psi_k(t; \boldsymbol{\eta}) = q_k(t) / \|q_k\|_2 \cdot \sqrt{v(t; \boldsymbol{\eta})} \quad (k \in \mathbb{N}, v \in \mathcal{V}, t \in \mathbb{R}).$$

Restrictions of \mathcal{V}

We consider nonnegative weight functions of the form

$$v(t; \boldsymbol{\eta}) = u(t; \boldsymbol{\eta}) \cdot w(t) = p_1(t; \boldsymbol{\eta}) / p_2(t; \boldsymbol{\eta}) \cdot e^{-t^2},$$

where p_1, p_2 are polynomials in t of degree ℓ, m such that $p_1/p_2 \geq 0$.

Weighted Hermite functions

Modification algorithms

- Due to the partial fraction decomposition of $u(t, \boldsymbol{\eta})$, it suffices to consider the factors $t - \eta_1$ and $(t - \eta_1)^2 + \eta_2^2$ and analogous divisors.
- Since the Hermite functions are defined over \mathbb{R} , only the following elementary modifications and their finite sums are allowed:

$$\begin{aligned} v_1(t; \eta_1) &:= u_1(t; \eta_1) \cdot w(t), & u_1(t; \eta_1) &:= (t - \eta_1)^2, \\ v_2(t; \boldsymbol{\eta}) &:= u_2(t; \boldsymbol{\eta}) \cdot w(t), & u_2(t; \boldsymbol{\eta}) &:= 1/((t - \eta_1)^2 + \eta_2^2), \\ & & (t \in \mathbb{R}, (\eta_1, \eta_2) \in \mathbb{R}^2, \eta_2 \neq 0, v_1, v_2 \in \mathcal{V}). \end{aligned}$$

Full problem (optimal weighting + affine trf.)

- $\Psi(\boldsymbol{\eta}; \boldsymbol{\tau}; \lambda)_{ik} := \Psi_k(t_i; \boldsymbol{\eta}; \boldsymbol{\tau}; \lambda) = \Psi_k(\lambda(t_i - \tau); \boldsymbol{\eta})$
- The extended variable projection problem can be written as:

$$\min_{\boldsymbol{\eta}, \boldsymbol{\tau}, \lambda} r_2(\boldsymbol{\eta}; \boldsymbol{\tau}; \lambda) = \min_{\boldsymbol{\eta}, \boldsymbol{\tau}, \lambda} \|\mathbf{f} - \Psi(\boldsymbol{\eta}; \boldsymbol{\tau}; \lambda) \Psi^+(\boldsymbol{\eta}; \boldsymbol{\tau}; \lambda) \mathbf{f}\|_2^2.$$

Weighted Hermite functions

Difficulties

- The system of weighted Hermite functions $\{\Psi_k(\cdot; \boldsymbol{\eta}) \mid k \in \mathbb{N}\}$ depends on the nonlinear parameters $\boldsymbol{\eta}$.
- Therefore, recomputing the corresponding recurrence coefficients $\hat{\alpha}_k(\boldsymbol{\eta})$ and $\hat{\beta}_k(\boldsymbol{\eta})$ for each value of $\boldsymbol{\eta}$ is a difficult task.

$$+ \qquad \qquad \qquad + \dots + \qquad \qquad \qquad =$$

Full problem: nonlinear LS approximation of a QRS complex using translated and dilated weighted Hermite functions.

Weighted Hermite functions

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Full problem: nonlinear LS approximation of a QRS complex using translated and dilated weighted Hermite functions (final optimization step).

Weighted Hermite functions

Idea

Reduce the full optimization problem to two simple sub-tasks.

Reduced problem

- 1 Instead of the full system, optimize the weight function only:

$$\min_{\boldsymbol{\eta}, \tau, \lambda} r_2(\boldsymbol{\eta}; \tau; \lambda) = \min_{\boldsymbol{\eta}, \tau, \lambda} \|\mathbf{f} - \sqrt{\mathbf{v}(\boldsymbol{\eta}; \tau; \lambda)}\|_2^2,$$

where $\mathbf{v}(\boldsymbol{\eta}; \tau; \lambda)_i := v(t_i; \boldsymbol{\eta}; \tau; \lambda) = v(\lambda(t_i - \tau); \boldsymbol{\eta})$.

- 2 Then, fix $\boldsymbol{\eta}$, and find the best affine parameters:

$$\min_{\tau, \lambda} r_2(\boldsymbol{\eta}; \tau; \lambda) = \min_{\tau, \lambda} \|\mathbf{f} - \boldsymbol{\Psi}(\boldsymbol{\eta}; \tau; \lambda) \boldsymbol{\Psi}^+(\boldsymbol{\eta}; \tau; \lambda) \mathbf{f}\|_2^2.$$

Weighted Hermite functions

Numerical optimization¹

- Projection operator: $\mathbf{P}_{\Psi(\boldsymbol{\eta})}^{\perp} := \mathbf{I} - \mathbf{P}_{\Psi(\boldsymbol{\eta})} = \mathbf{I} - \boldsymbol{\Psi}(\boldsymbol{\eta})\boldsymbol{\Psi}^+(\boldsymbol{\eta})$.
- For the sake of simplicity, we omit the vector of free parameters $\boldsymbol{\eta}$ from the notations. Then, the j th coordinate of the gradient is

$$\frac{1}{2}\nabla r_2^{(j)} = \left(- \left(\mathbf{P}_{\Psi}^{\perp} \mathbf{D}_j \boldsymbol{\Psi}^+ + (\mathbf{P}_{\Psi}^{\perp} \mathbf{D}_j \boldsymbol{\Psi}^+)^T \right) \mathbf{f} \right)^T \mathbf{P}_{\Psi}^{\perp} \mathbf{f},$$

where $\mathbf{D}_j := \partial \boldsymbol{\Psi}(\boldsymbol{\eta}) / \partial \eta_j$.

- It can be calculated only for the affine and the reduced problem.
- In case of the full problem, quasi-Newton methods can be used.

¹G. H. Golub and V. Pereyra, *The differentiation of pseudo-inverses and nonlinear least squares problems whose variables separate*, SIAM Journal on Numerical Analysis (SINUM), vol. 10, pp. 413–432, 1973.

Constraining the optimization

Parameters of $u_1(t; \eta) = (t - \eta)^2$

If η is far from zero, u_1 is smoothed out by the tails of $w(t) = e^{-t^2}$. Since w is a Gaussian, the three-sigma rule applies with $\sigma = 1/\sqrt{2}$. Therefore, we restrict the values of η to the interval $[-3\sigma; 3\sigma]$.

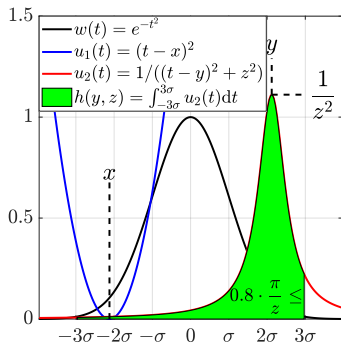
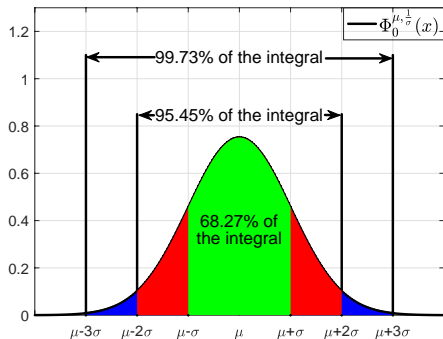
Parameters of $u_2(t; \eta) = 1/((t - \eta_1)^2 + \eta_2^2)$

Choose η such that the following inequality is satisfied:

$$0.8 \cdot \int_{-\infty}^{\infty} u_2(t; \eta) dt \leq \int_{-3\sigma}^{3\sigma} u_2(t; \eta) dt.$$

It means that the main lobe of u_2 cannot be too wide, i.e., 80% of its overall integral should lie in the interval $[-3\sigma; 3\sigma]$.

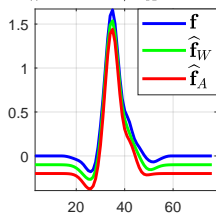
Constraining the optimization



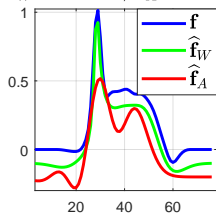
The three-sigma rule and the constraints.

Weighted Hermite functions - Illustrations

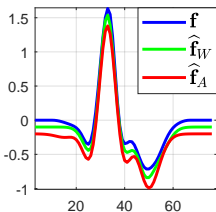
$e_W = 2.7\%$, $e_A = 4.4\%$



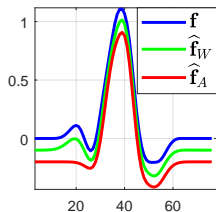
$e_W = 11.3\%$, $e_A = 33.7\%$



$e_W = 5.6\%$, $e_A = 8.5\%$



$e_W = 2.8\%$, $e_A = 9.0\%$



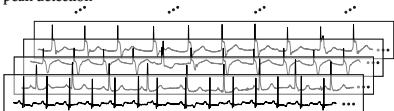
Examples using 6 basis functions for which the affine Hermite model (red line) does not work perfectly, the weighted Hermite model (green line) performs better.

Experiments

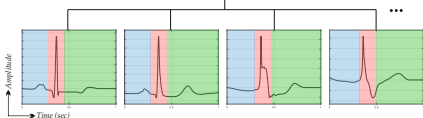
Evaluation method and data

- ECG data compression.
- Good benchmark regarding the distortion of ECG signals.
- 12 hours of ECG raw data from MIT/BIH arrhythmia database.

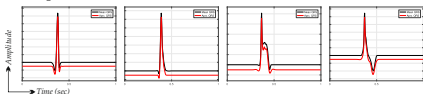
1) R peak detection



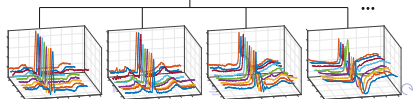
2) Slice and calculate mean beats, split in three segments



3) Two - step optimization approach to determine individual initial free parameters



4) Slice single beats and optimize affine parameters for P-QRS-T



Experiments cont.

Evaluation method and data

- ECG data compression
- Good benchmark regarding the distortion of ECG signals
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Comparison to other work

- Compression ratio
- Normalized PRDN for M ECG beats / QRS complexes

$$\overline{\text{PRDN}} = 100 \cdot \frac{1}{M} \sum_{m=1}^M \frac{\|\mathbf{f}_m - \hat{\mathbf{f}}_m\|_2}{\|\mathbf{f}_m - \bar{\mathbf{f}}_m\|_2},$$

- Dilation only vs. affine transformation vs. our work

Results

Experimental results of 12 hours long real ECG data.

Rec.	Dilation only ¹			Affine trf. ²			Proposed work			System
	PRDN	QRS PRDN	CR	PRDN	QRS PRDN	CR	PRDN	QRS PRDN	CR	
mean	18.18	20.28	19.75	15.40	11.40	18.83	14.88	9.86	18.82	-
Selected recordings (for illustration)										
100	17.09	16.57	19.47	13.09	12.09	18.52	9.78	7.74	18.52	qf
102	33.57	36.34	20.22	33.69	24.91	19.23	31.27	16.05	19.23	qd
104	31.94	39.49	19.96	34.10	37.57	18.98	29.78	20.38	18.98	qd
232	32.40	20.28	24.39	26.00	14.55	23.22	24.18	9.59	23.21	qd+qf

¹R. Jané, S. Olmos, P. Laguna, and P. Caminal, *Adaptive Hermite models for ECG data compression: performance and evaluation with automatic wave detection*, in Proc. of Computers in Cardiology Conference, 1993, pp. 389–392.

²T. Dózsa and P. Kovács, *ECG signal compression using adaptive Hermite functions*, Advances in Intelligent Systems and Computing, vol. 399, pp. 245–254, 2015.

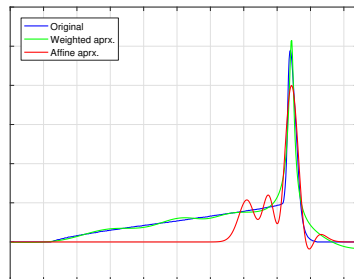
Conclusions and applications

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- Generalization of former wave shape models allowing to model more complex wave forms
- Preoptimized parameters \rightarrow subject-specific.
- \mathbf{c} , τ , $\lambda \rightarrow$ morphological changes over time.

Applications

- Signal classification and detection, information extraction.
- Potentially suitable for modeling action potentials, blood pressure, or other biomedical signals.



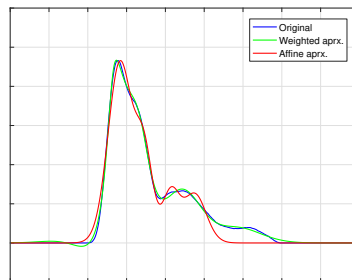
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Conclusions cont.

Advantages compared to PCA, DWT, etc.

- Method works for ECG recordings of any size (PCA not suited for short recordings).
- Domain of translation / dilation is continuous \rightarrow resampling at any grid is possible.
- Wide field of applications (biomedical / image / radar signal processing, computer tomography, physical optics, ...).
- Automatic separation of morphological changes induced by translation (τ), dilation (λ), or other sources (e.g. change of amplitude \rightarrow c). Methods like PCA lack this ability.

Separation of morphological changes

Translation

Morphological changes induced by the translation of a wave (e.g. due to changing heart rate) are captured by τ .





Dilation

Morphological changes induced by the dilation of a wave are captured by λ .





Additional Morphological changes

Morphological changes which are not induced by translation or dilation but other (possibly diagnostic) sources, should be captured by c .




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