Nuclei Segmentation in Histopathology Images

Deniz Mercadier Sayın*, <u>Beril Besbinar</u>[†], Pascal Frossard[†] May 16, 2019

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Why histopathology images?

• Common practice of digital pathology

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• Common practice of digital pathology Hematoxylin and Eosin (H&E) stain is one of the principal stains



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What are the challenges?

- Variation of nuclear size and shape
- Variations in staining techniques



Existing Methods

Traditional approaches

- (Optional) Pre-processing/color normalization
- Feature extraction (color, texture, shape-based)
- Pixel-wise classifier or watershed/graph-cut
- \cdot (Optional) Post-processing for cluttered nuclei

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Deep Learning (DL) approaches

- (Optional) Pre-processing/color normalization
- Pixel-wise classification using the patches around pixels Merging two tasks have already improved the performance
- \cdot (Optional) Post-processing for cluttered nuclei

Classification at each pixel

 $\label{eq:classification} \begin{array}{l} \text{Classification at each pixel} \leftarrow \\ \text{Final mask is obtained via a sliding window} \end{array}$

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- Dataset: Partially annotated dataset introduced in Janowczyk et al.
- Adaptation of loss function to partially annotated dataset
- Architecture: U-Net (with modifications)

The dataset introduced in [1]: 141 Hematoxylin and Eosin (H&E) stained images

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- of size 2000 x 2000
- at 40x magnification
- with partial annotations.

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labels: $y_{ij} \in \{0,1\}$ $\begin{cases} y_{ij} = 1 : \text{nuclei} \\ y_{ij} = 0 : \text{non-nuclei/not-annotated} \end{cases}$

predicted labels:
$$\hat{y}_{ij}^{\text{fg}}, \hat{y}_{ij}^{\text{bg}} \in [0, 1], \quad \hat{y}_{ij} = \begin{cases} 1 & \text{if} \quad \hat{y}_{ij}^{\text{fg}} \ge \hat{y}_{ij}^{\text{bg}} \\ 0 & \text{if} \quad \hat{y}_{ij}^{\text{fg}} < \hat{y}_{ij}^{\text{bg}} \end{cases}$$

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$$\mathcal{L} = \sum_{(i,j) \in WxH} y_{ij} \log \hat{y}_{ij}^{\text{fg}} + (1 - y_{ij}) \log \hat{y}_{ij}^{\text{bg}}$$

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$$d_{ij} = \min_{\substack{\{i,j\}, (u,v) \in WxH \\ \{(i,j) \mid y_{ij}=1\}}} (\sqrt{(i-u)^2 + (j-v)^2})$$
$$m_{ij} = \begin{cases} 1, & \text{if } d_{ij} \le \alpha \\ e^{-\beta(d_{ij}-\alpha)}, & \text{if } d_{ij} > \alpha \end{cases}$$

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$$\begin{split} d_{ij} &= \min_{\substack{(i,j), (u,v) \in WxH \\ \{(i,j) \mid y_{ij}=1\}}} (\sqrt{(i-u)^2 + (j-v)^2}) \\ m_{ij} &= \begin{cases} 1, & \text{if } d_{ij} \leq \alpha \\ e^{-\beta(d_{ij}-\alpha)}, & \text{if } d_{ij} > \alpha \end{cases} \end{split}$$

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b is obtained via unsupervised clustering k-means (k=2) using H,E,D channels:

	OD_B	OD_G	OD_R
Hematoxylin	0.08	0.20	0.18
Eosin	0.01	0.13	0.01
DAB	0.29	0.21	0.10

[4] Ruifrok, A. C., and Johnston, D. A., "Quantification of histochemical staining by color deconvolution" Analytical and quantitative cytology and histology the International Academy of Cytology [and] American Society of Cytology, 2001.

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Method - Architecture

U-Net with 4 convolutional-deconvolutional layers



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Architecture search:

- Different numbers of convolutional/deconvolutional layers
- Different numbers of filter sizes
- Different activation functions

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Modifications:

- Zero-padded convolutions for input size flexibility
- Batch normalization

• Split of 121/5/15 for training, validation and testing

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- Elimination of 'uninformative' patches
 - # foreground pixels < 10% # total pixels
 - # background pixels < 40% # total pixels

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- Data augmentation: rotation, flip, elastic deformation

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71842 total number of patches





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Experiments - Additional Datasets

DS1 [3]: 50 H&E images of size 500 x 500, from 11 different patients with breast cancer

- pp: per patient, all: all images/patients

[3] Naylor, P., Laé ,M., Reyal, F., and Walter, T., "Segmentation of nuclei in histopathology images by deep regression of the distance map,"IEEE Transactions on Medical Imaging, 2018

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- breast, liver, kidney, prostate, bladder, colon, stomach

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! No fine tuning before testing the models on the new datasets

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$$G = \bigcup_{i=1}^{K} G_i$$
 GT nuclei pixels, $P = \bigcup_{j=1}^{L} P_j$ predicted nuclei pixels

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			Recall	Precision	F1 score	Accuracy	JI (IoU)	AJI	Time (sec)
	0	[1]	0.35 (0.21)	0.91 (0.06)	0.45 (0.21)	0.92 (0.02)	0.32 (0.18)	0.84 (0.04)	467.88 (13.67)
	d	Proposed	0.60 (0.14)	0.89 (0.04)	0.70 (0.10)	0.94 (0.02)	0.55 (0.11)	0.88 (0.03)	0.47 (0.01)
DS	all	[1]	0.33 (0.23)	0.92 (0.08)	0.44 (0.23)	0.92 (0.06)	0.31 (0.20)	0.85 (0.10)	467.88 (13.67)
		Proposed	0.60 (0.17)	0.90 (0.06)	0.70 (0.13)	0.94 (0.04)	0.55 (0.14)	0.89 (0.08)	0.47 (0.01)
DS 2		[1]	0.59 (0.23)	0.81 (0.15)	0.63 (0.18)	0.85 (0.08)	0.49 (0.17)	0.70 (0.14)	1642.99 (39.91)
		Proposed	0.73 (0.16)	0.82 (0.09)	0.76 (0.12)	0.89 (0.06)	0.62 (0.13)	0.78 (0.10)	1.84 (0.06)

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0.81 mean F1, 0.56 mean AJI 0.81 mean F1, 0.57 mean AJI

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MoNuSeg Challenge @ MICCAI 2018 (trained with DS2): Top three performing algorithms: 0.6907, 0.6868, 0.6852 mean AJI

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- We proposed a method for nuclei segmentation in histapathology images using incomplete ground truth information
- Incorporation of prior knowledge, even with uncertainty, helps us to design more efficient models/algorithms
- Pixel-based processing for holistic tasks is not efficient
- There exists an open-source plug&play model for nuclei segmentation: at least a point you can start with

Questions?

Deniz Mercadier Sayın*, <u>Beril Besbinar</u>[†], Pascal Frossard[†] **beril.besbinar@epfl.ch** [†]EPFL - Signal Processing Laboratory (LTS4)



Evaluation Metrics

Pixel-based Evaluation Metrics:

TN: True Negative TP: True Positive FN: False Negative FP: False Positive

Predicted

		Negative	Positive
Actual	Negative	ΤN	FP
	Positive	FN	TP

$$recall = \frac{TP}{TP + FN} \qquad F1 \text{ score} = 2 * \frac{\text{precision} * \text{recall}}{\text{precision} + \text{recall}}$$
$$precision = \frac{TP}{TP + FP} \qquad \text{accuracy} = \frac{TP + TN}{TP + TN + FP + FN}$$
$$Jaccard Index (JI) = \frac{TP}{TP + FN + FP}$$

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Final Mask Generation



For an 2000x2000 image

- patches of size 256x256:
 256 patches
- pixel-based processing by patches of size 32x32: ≈ 3.88m patches

Quantitative Analysis

			Recall	Precision	F1 score	Accuracy	JI (IoU)	AJI	Time (sec)
DS 1	dd	[1]	0.35 (0.21)	0.91 (0.06)	0.45 (0.21)	0.92 (0.02)	0.32 (0.18)	0.84 (0.04)	467.88 (13.67)
		Proposed	0.60 (0.14)	0.89 (0.04)	0.70 (0.10)	0.94 (0.02)	0.55 (0.11)	0.88 (0.03)	0.47 (0.01)
	all	[1]	0.33 (0.23)	0.92 (0.08)	0.44 (0.23)	0.92 (0.06)	0.31 (0.20)	0.85 (0.10)	467.88 (13.67)
		Proposed	0.60 (0.17)	0.90 (0.06)	0.70 (0.13)	0.94 (0.04)	0.55 (0.14)	0.89 (0.08)	0.47 (0.01)
DS 2		[1]	0.59 (0.23)	0.81 (0.15)	0.63 (0.18)	0.85 (0.08)	0.49 (0.17)	0.70 (0.14)	1642.99 (39.91)
		Proposed	0.73 (0.16)	0.82 (0.09)	0.76 (0.12)	0.89 (0.06)	0.62 (0.13)	0.78 (0.10)	1.84 (0.06)

		F1	AJI
DS 1	[2]	0.72	0.54
	[3] trained with DS2	0.81	0.56
	[3] trained with DS1 & DS2	0.81	0.57
	[3] trained only on Breast	0.82	0.59

MoNuSeg Challenge @ MICCAI 2018 (trained with DS2):

Top three performing algorithms: 0.6907, 0.6868, 0.6852 mean AJI

[1] Janowczyk, A., and Madabhushi, A., "Deep learning for digital pathology image analysis: A comprehensive tutorial with selected use cases," Journal of pathology informatics, 2016.

[2] Kumar, N., Verma, R., Sharma, S., Bhargava, S., Vahadane, A., and Sethi, A.,"A dataset and a technique for generalized nuclear segmentation for computational pathology,"IEEE transactions on medical imaging, 2017.
[3] Naylor, P., Laé, M., Reyal, F., and Walter, T., "Segmentation of nuclei in histopathology images by deep regression of the distance map."IEEE transactions on Medical Imaging, 2018

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Experiments - Qualitative Analysis



Proposed method

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