



# DEEP NEURAL NETWORK BASED COUGH DETECTION USING BED-MOUNTED ACCELEROMETER MEASUREMENTS

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ICASSP 2021

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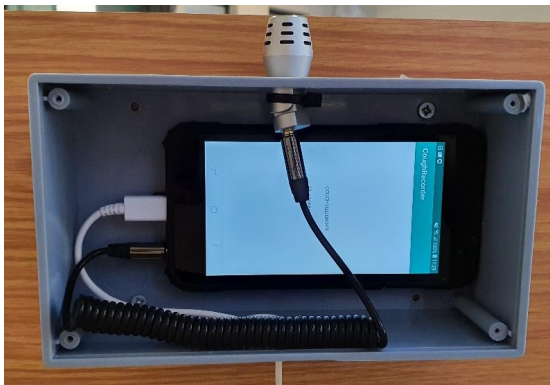
- It is noninvasive.
- It is less intrusive than body-attached accelerometer sensors.
- It sidesteps privacy concerns encountered when using audio for cough detection.
- Thus it is as an excellent tool for long-term cough monitoring.

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# Introduction

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- Previously, body-attached accelerometers have been used to detect movements including coughs with high accuracy.
- However, attaching an accelerometer to the patient's body is inconvenient and intrusive. Thus, we propose the monitoring of coughing based on the signals obtained from the accelerometer integrated into an inexpensive consumer smartphone firmly attached to the patient's bed, thereby eliminating the need to wear a measuring equipment.



**A Samsung Galaxy J4  
smartphone with an inbuilt  
accelerometer connected to  
an external BOYA BY-MM1  
cardioid microphone by a  
3.5 mm audio jack**



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- In addition, continuous video recordings were made using ceiling-mounted cameras in order to ensure accurate data annotation.

**Table: Ground Truth Dataset Summary:** ‘PATIENTS’: list of the patients; ‘COUGHS’: number of cough events; ‘NON COUGHS’: number of events that are not coughs; ‘COUGH TIME’: total amount of time (in sec) for cough events; ‘NON-COUGH TIME’: total amount of time (in sec) for non-cough events.

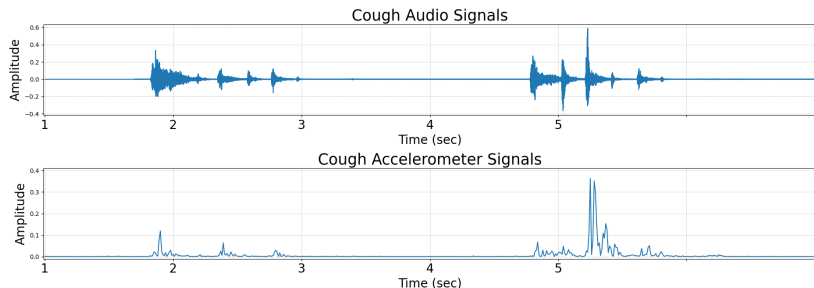
PATIENTS	COUGHS	NON COUGHS	COUGH TIME	NON- COUGH TIME
Patient 1	88	973	169.16	1660.67
Patient 2	63	1111	117.67	1891.92
Patient 3	469	11025	893.91	18797.32
Patient 4	109	9151	204.06	15596.71
Patient 5	97	7826	188.26	13344.98
Patient 6	192	12437	360.72	21197.35
Patient 7	436	14053	825.23	23953.15
Patient 8	368	2977	702.05	5077.89
Patient 9	2816	3856	5345.27	6569.32
Patient 10	649	2579	1236.84	4400.42
Patient 11	205	527	391.42	901.38
Patient 12	213	323	402.61	547.62
Patient 13	213	712	401.61	1211.75
Patient 14	82	455	158.77	777.64
<b>TOTAL</b>	<b>6000</b>	<b>68005</b>	<b>11397.6</b>	<b>115928.12</b>

- Our ground truth dataset contains 6000 coughs and 68000 non-coughs from 14 adult male patients totalling 3.16 and 32.20 hours of data respectively. No other information regarding patients are recorded due to ethical constraints.

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- Coughs are underrepresented in our dataset and to compensate this imbalance, we have applied SMOTE data balancing during training.

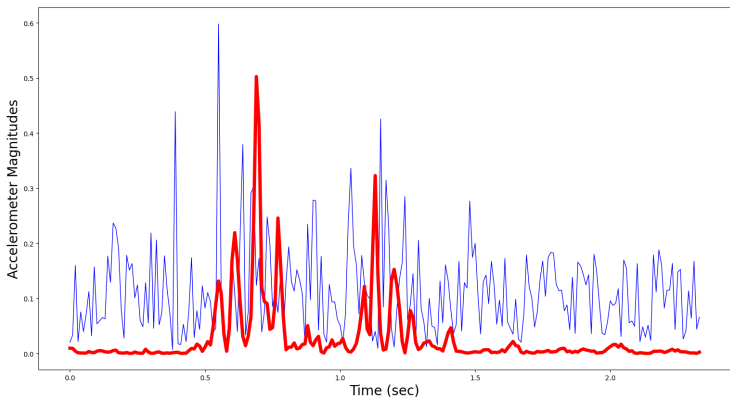
# Cough Audio & Accelerometer Signal

- Coughs are very distinctive in nature.
- The following figure shows the audio and accelerometer signals two consecutive coughs from a patient and the unique patterns in both audio and accelerometer measurements.



# Cough & Non-cough Accelerometer Signal

- Example accelerometer magnitudes for a cough and a non-cough event



# Feature Extraction

- Power spectra, root mean square amplitude, kurtosis, moving average and crest factor are extracted from the acceleration signals as features for cough detection.

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Hyperparameter Description	Range
• Size of frames in samples in which cough is segmented ( $\Psi$ )	$2^k$ where $k = 4, 5, 6$
Number of segments in which frames were grouped ( $C$ )	5, 10

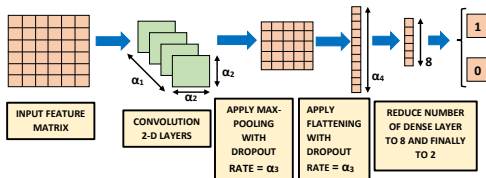
- The input feature matrix has the dimension of  $(C, \frac{\Psi}{2} + 5)$  and power spectra have  $(\frac{\Psi}{2} + 1)$  coefficients.



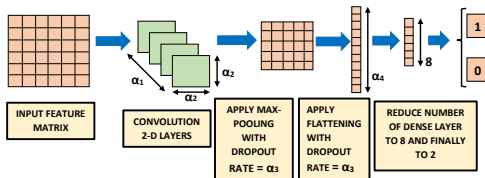
- Only CNN and LSTM has their hyperparameters optimised. The default 50 layer residual architecture used as Resnet50.

Hyperparameters	Range
No. of Conv filters ( $\alpha_1$ )	$3 \times 2^k$ where $k = 3, 4, 5$
kernel size ( $\alpha_2$ )	2 and 3
Dropout rate ( $\alpha_3$ )	0.1 to 0.5 in steps of 0.2
• Dense layer size ( $\alpha_4$ )	$2^k$ where $k = 4, 5$
LSTM units ( $\beta_1$ )	$2^k$ where $k = 6, 7, 8$
Learning rate ( $\beta_2$ )	$10^k$ where $k = -2, -3, -4$
Batch Size ( $\xi_1$ )	$2^k$ where $k = 6, 7, 8$
No. of epochs ( $\xi_2$ )	10 to 200 in steps of 20

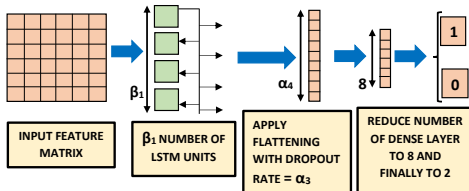
- CNN architecture showing hyperparameters



- CNN architecture showing hyperparameters



- LSTM architecture showing hyperparameters



- The best results from these three classifiers:

<b>Clas- -sifier</b>	<b>Frame (<math>\Psi</math>)</b>	<b>Seg (<math>C</math>)</b>	<b>Mean Spec</b>	<b>Mean Sens</b>	<b>Mean Accuracy</b>	<b>Mean AUC</b>
CNN	64	10	91%	80%	86%	0.9499
LSTM	32	10	86%	93%	89%	0.9572
<i>Resnet50</i>	<i>32</i>	<i>10</i>	<i>94%</i>	<i>99%</i>	<i>97%</i>	<i>0.9888</i>

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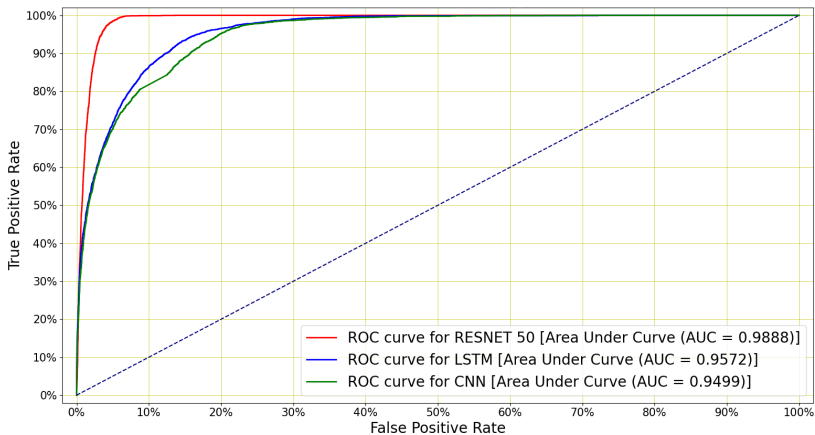
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- AUC values are averaged over 14 leave-one-patient-out cross-validation folds during hyperparameter optimisation.
- The best performance is achieved by the Resnet50 architecture, with an AUC of 0.9888 after 50 epochs at training when using 32 sample (320 msec) long frames and 10 segments.

# Results



**Figure: Mean ROC curves**, for the best performing classifiers. Resnet50 outperforms the LSTM and CNN over a wide range of operating points.

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- This type of monitoring is less intrusive than approaches in which the accelerometer is attached to the body.
- It therefore presents a promising approach to the long-term cough monitoring, which can be of practical use in monitoring the recovery process of patients, for example in the clinic where the data was collected.