Unrolled Projected Gradient Algorithm for Stain Separation in Digital Histopathological Images

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- **2** Problem formulation
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- 4 Results
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Introduction	Introduc	tion			

Histopathological images

Staining the tissue of a given organ using a combination of color dyes

- Hematoxylin (H): bluish-purple stain strongly related to the nuclei.
- Eosin (E): red-pink stain that highlights the cytoplasm of the nucleus.
- Saffron (S): yellow stain used to detect connective tissues.



Figure 1: Example of HES-stained image.

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Challenge: Variation in staining protocols

- Digital histopathological images, particularly HES-stained images, suffer from color variations due to differences in staining protocols, and materials.
- These color variations affect the accuracy of computer-aided systems used for disease diagnosis, especially in cancer detection.

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- Digital histopathological images, particularly HES-stained images, suffer from color variations due to differences in staining protocols, and materials.
- These color variations affect the accuracy of computer-aided systems used for disease diagnosis, especially in cancer detection.
- Need for the standardization/normalization of the different stain appearances to ensure consistent results.





(b)

(d)

Figure 2: The principle of stain separation: (a) HES-stained image. (b) H-stained image. (c) E-stained image. (d) S-stained image.

(c)





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Figure 2: The principle of stain separation: (a) HES-stained image. (b) H-stained image. (c) E-stained image. (d) S-stained image.

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Contribution

- State-of-the-art methods: SVD, ICA and NMF
- Traditional stain separation methods often require image-specific parameter tuning, which is set in an empirical manner and computationally expensive.





(d)

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Contribution

- State-of-the-art methods: SVD, ICA and NMF
- Traditional stain separation methods often require image-specific parameter tuning, which is set in an empirical manner and computationally expensive.
- Goal: design an efficient and robust stain separation method, and enable supervised learning of the hyperparameters



(a)

(c)

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- Traditional stain separation methods often require image-specific parameter tuning, which is set in an empirical manner and computationally expensive.

Goal: design an efficient and robust stain separation method, and enable supervised learning of the hyperparameters

 \rightarrow Main ideas: Projected Gradient algorithm and unrolling paradigm

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Problem	formulation			

Beer-Lambert law [1]

$$I = I_0 \cdot \exp(-WH)$$

$$\implies_{\text{ptical Density}} \quad V = -\log\left(\frac{I}{I_0}\right)$$

(1)

$$V = WH$$

0

• $I \in \mathbb{R}^{3 \times N}$: vectorized HES-stained image

- *I*₀: incident light intensity
- $V \in \mathbb{R}^{3 \times N}$: Optical Density (OD) version of *I*
- $W \in \mathbb{R}^{3 \times r}$: stain-color vector matrix (can be experimentally estimated)
- $H \in \mathbb{R}^{r \times N}$: stain concentration matrix
- N is the image size
- *r* is the number of stains

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- N is the image size
- *r* is the number of stains

• Goal: Estimate *H* given an observed *V* and a known *W*.

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Problem 1	formulation			

Equation (1) can be solved by formulating the following optimization problem:

$$\begin{array}{l} \underset{H \in \mathbb{R}^{r \times N}}{\text{minimize}} \quad \frac{1}{2} \|V - WH\|_{\mathrm{F}}^{2} + R(H) \\ \text{subject to} \quad H \ge 0 \end{array}$$
(2)

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Problem (2) can be rewritten as follows:



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• The Regularization term *R* is given by

$$R(H; \lambda_1, \lambda_2, \varepsilon) = \underbrace{\frac{\lambda_1}{2} \|H\|_{\mathrm{F}}^2}_{\text{quadratic term}} + \underbrace{\lambda_2 \sum_{c=1}^r \sum_{i=1}^N \sqrt{(D_v H_c^\top)_i^2 + (D_h H_c^\top)_i^2 + \varepsilon^2}}_{\text{smoothed total variation (STV)}}$$
(4)

where λ_1 and λ_2 are positive regularization parameters, ε is the STV parameter and, $D_{\nu} \in \mathbb{R}^{N \times N}$ and $D_h \in \mathbb{R}^{N \times N}$ are the vertical and horizontal discrete gradient operators, respectively.

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Problem for	ormulation			

Our minimization problem can be seen as the minimization of two functions g and f

$$\underset{H \in \mathbb{R}^{r \times N}}{\text{minimize}} \quad \underbrace{\frac{1}{2} \|V - WH\|_{\mathrm{F}}^{2} + R(H; \lambda_{1}, \lambda_{2}, \varepsilon)}_{g(H; \lambda_{1}, \lambda_{2}, \varepsilon)} + \underbrace{\iota_{[0, +\infty[r \times N]}(H)}_{f(H)} \tag{5}$$

- f and g are proper lower-semicontinuous convex functions on $\mathbb{R}^{r \times N}$
- g is differentiable with an L-Lipschitzian gradient with respect to H.
- *f* is a function whose proximity operator reduces to the projection $\operatorname{proj}_{[0,+\infty[^{r\times N}]}$ onto the nonnegative orthant $[0,+\infty[^{r\times N}]$.

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- f and g are proper lower-semicontinuous convex functions on $\mathbb{R}^{r \times N}$
- *g* is differentiable with an *L*-Lipschitzian gradient with respect to *H*.
- *f* is a function whose proximity operator reduces to the projection $\operatorname{proj}_{[0,+\infty[^{r\times N})}$ onto the nonnegative orthant $[0,+\infty[^{r\times N})$.
- Problem (5) can be solved using Projected Gradient Algorithm (PGA), which is a special case of the proximal gradient algorithms [2].

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Optimizati	ion algorithm			

Algorithm 1 Projected Gradient Algorithm (PGA)

Input: Initial point $H_0 \in \mathbb{R}^{r \times N}$, fixed stepsize $\gamma \in [0, \frac{2}{L}]$ and number of iterations $K \in \mathbb{N}^*$. **for** $k = 0, 1, \dots, K - 1$ **do** $H_{k+1} = \operatorname{proj}_{[0, +\infty[^{r \times N}]} (H_k - \gamma \nabla g(H_k; \lambda_1, \lambda_2, \varepsilon))$ **end for**

where *L* is the Lipschitz constant of the gradient ∇g given by

$$L = \|W\|_{\mathrm{S}}^2 + \lambda_1 + 8\frac{\lambda_2}{\varepsilon}.$$

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Optimizati	ion algorithm			

Algorithm 2 Projected Gradient Algorithm (PGA)

Input: Initial point $H_0 \in \mathbb{R}^{r \times N}$, fixed stepsize $\gamma \in [0, \frac{2}{L}[$ and number of iterations $K \in \mathbb{N}^*$. **for** $k = 0, 1, \dots, K - 1$ **do** $H_{k+1} = \operatorname{proj}_{[0, +\infty[^{r \times N}]} (H_k - \gamma \nabla g(H_k; \lambda_1, \lambda_2, \varepsilon))$ **end for**

where *L* is the Lipschitz constant of the gradient ∇g given by

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Difficulty

Hyperparameters setting $(\gamma, \lambda_1, \lambda_2, \epsilon)$

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Unrolled	PGA			

Advantages

- Deployment of a neural network architecture.
- Learning the hyperparameters from a training dataset.
- Interpretable and flexible algorithm.
- Reducing the required number of iterations (faster convergence).



One layer \mathcal{L}_k of the Unrolled PGA mirrors one iteration for PGA by

$$\begin{aligned} H_{k+1} &= \operatorname{proj}_{[0,+\infty[^{r \times N}} \left(H_k - \gamma_k \nabla g(H_k;\lambda_{1,k},\lambda_{2,k},\varepsilon_k) \right) \\ &= \operatorname{proj}_{[0,+\infty[^{r \times N}} \left(H_k - \gamma_k(A(H) + B(H;\lambda_{1,k}) + C(H;\lambda_{2,k},\varepsilon_k)) \right) \end{aligned}$$
(6)



Figure 3: Unrolled PGA architecture.

where,

- $A(H) = W^{\top}(WH V)$
- $B(H; \lambda_{1,k}) = \lambda_{1,k}H$
- $C(H; \lambda_{2,k}, \varepsilon_k) = \nabla STV(H; \lambda_{2,k}, \varepsilon_k)$

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Unrolled]	PGA			

Hyperparameters learning

To obtain the vector of parameters $\Theta_k = [\lambda_{1,k}, \lambda_{2,k}, \varepsilon_k, \gamma_k]^{\top}$, and ensure its positivity, we consider:

$$\forall k \in \{0, .., K-1\} \quad \Theta_k = \text{Softplus}(\Psi_k), \tag{7}$$

where Ψ_k is a vector of parameters learned during the training.



Figure 4: Unrolled PGA architecture with parameters learning.

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Loss function

The resulting neural network architecture is trained by minimizing:

$$\mathcal{L}(\Theta) = \frac{1}{3} \sum_{c \in \{h, e, s\}} \ell(I_c^{(GT)}, I_c(\Theta)),$$
(8)

where

- $\Theta = (\Theta_k)_{0 \le k \le K-1}$ represents the global set of parameters
- ℓ is a given criterion used to compare the reconstructed image I_c associated to the stain c with its corresponding ground truth $I_c^{(GT)}$.

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Experimen	ntal settings			

- Our data was acquired at the Kremlin-Bicêtre hospital, France.
- The unrolled PGA was composed of 20 layers ⇒ 80 trainable parameters.
- Our model is implemented in Pytorch, using the ADAM optimizer with an initial learning rate set to 0.01.
- The batch size and number of epochs were set to 5 and 150, respectively.

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Numerica	l results			

Table 1: Stain separation performance.

	PSNR	SSIM	PieAPP
Ruifrok and Johnston [3]	44.841	0.355	2.134
Xu et al. [4]	44.315	0.369	1.979
Vahadane et al. [5]	42.220	0.368	1.851
Yang et al. [6]	42.755	0.355	1.841
PGA	45.254	0.394	1.477
Unrolled PGA	46.525	0.427	1.161

Key observations: PGA and Unrolled PGA vs SOA Methods

- Both PGA and Unrolled PGA demonstrated superior performance compared to the SOA methods.
- The Unrolled PGA outperformed all methods across all metrics.



Figure 5: Illustration of the separated stain images (3 examples). 1st row: Ground truth. 2nd row: Xu *et al.* [4]. 3rd row: Vahadane *et al.* [5]. 4th row: Yang *et al.* [6]. 5th row: PGA. Last row: unrolled PGA.

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Conclusion

- Designing an iterative projected gradient algorithm for the stain separation problem.
- ✓ Incorporating smooth total variation regularization to improve the quality of separation.
- ✓ Unrolling the algorithm into a neural network architecture
- ✓ The proposed method demonstrated significant objective improvements, in terms of PSNR, SSIM, and PieAPP, over state-of-the-art methods.
- ✓ Subjective evaluations showed that our approach produced visually superior results in stain separation.

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Perspectives

- Extending the optimization problem to estimate both the matrices W and H simultaneously
- Going beyond stain separation to tackle stain normalization as well as other potential applications

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