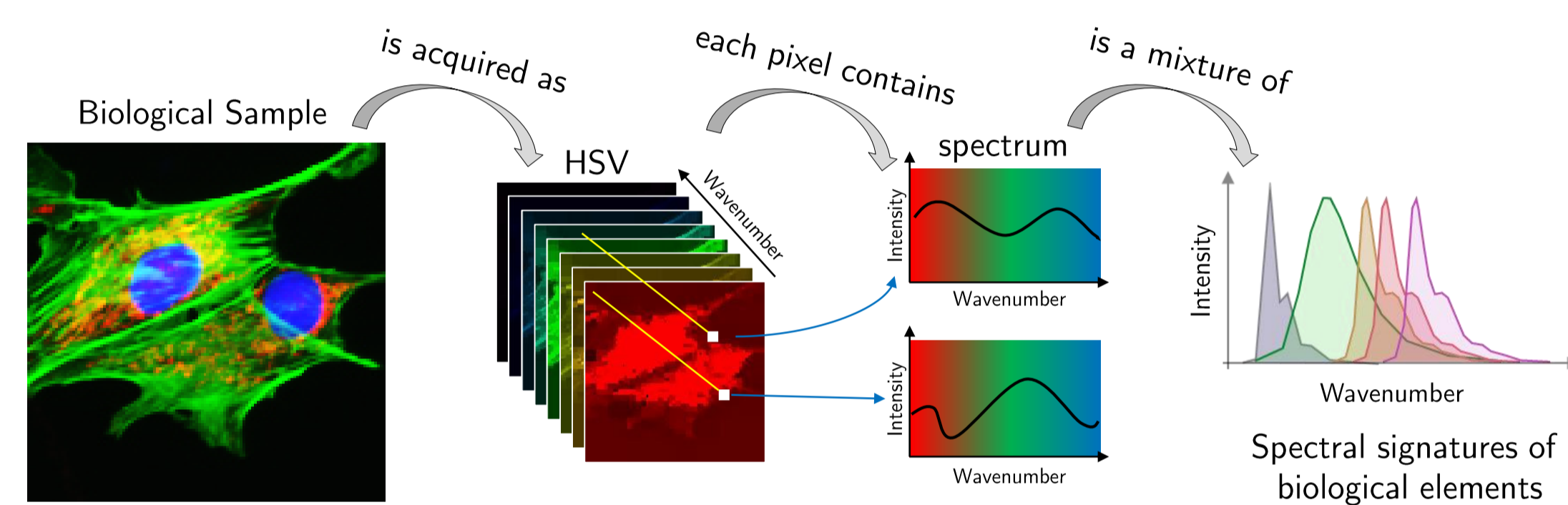


## 1. Summary

- **Motivations:** Acquisition of biological HyperSpectral Volume (HSV).
  - ✓ FTI reaches high spectral resolution without reducing SNR (see below).
  - ✗ Higher resolution  $\Rightarrow$  longer exposure time  $\Rightarrow$  more photo-bleaching.
- **Contribution:** Resorting to the theory of Compressed Sensing (CS) to
  - ▷ design an optimum light coding scheme,
  - ▷ reduce light exposure  $\Rightarrow$  less photo-bleaching,
  - ▷ provide a robust and stable HS recovery guarantee.

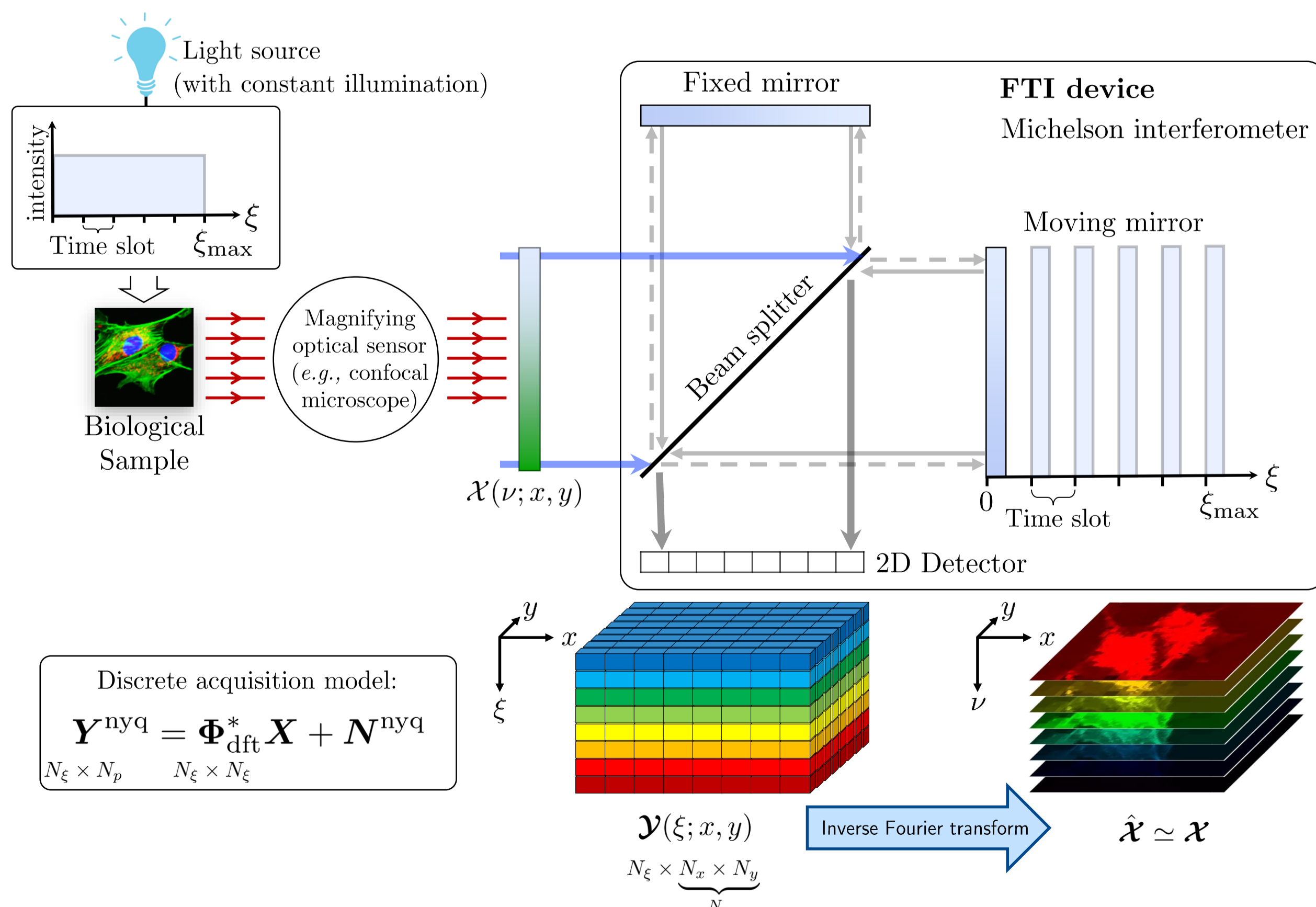
## 2. What is a Biological Hyperspectral Volume?

The description of a biological sample both by its spatial and spectral content, with the purpose of distinguishing specific biological elements, as in fluorescence spectroscopy.



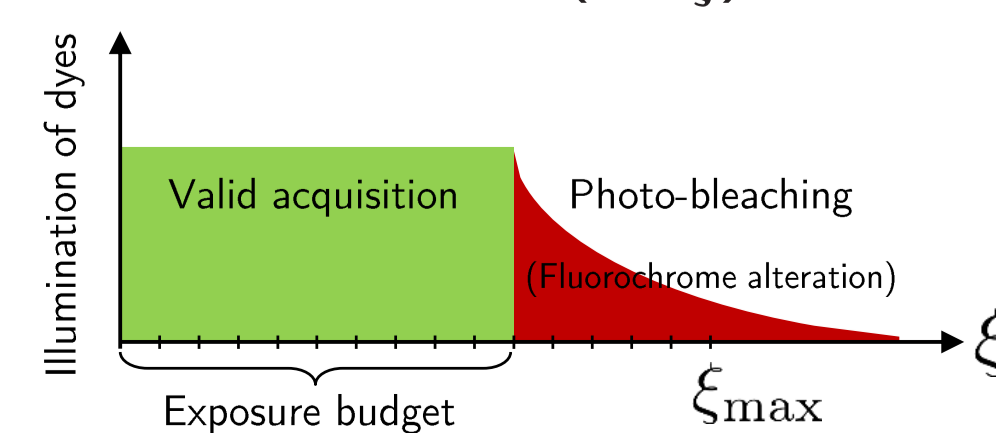
## 3. Nyquist Fourier Transform Interferometry (FTI)

- **Mechanism:**
  - ▷ For each Optical Path Difference (OPD) 2D focal plane measurements are recorded.
  - ▷ An *inverse 1D Fourier transform* is applied along the OPD axis to achieve the HSV.



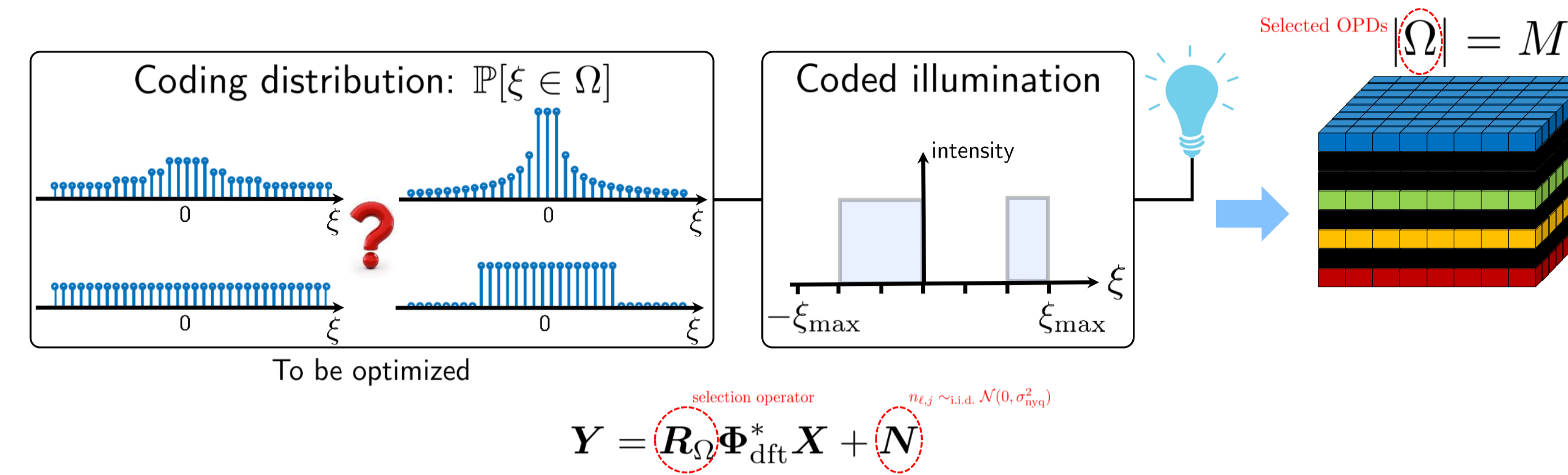
- **Pros & cons:** As the number of recorded OPD points ( $N_\xi$ ) increases,

- ✓ the spectral resolution increases.
- ✗ the specimen is over-exposed  $\Rightarrow$  more photo-bleaching

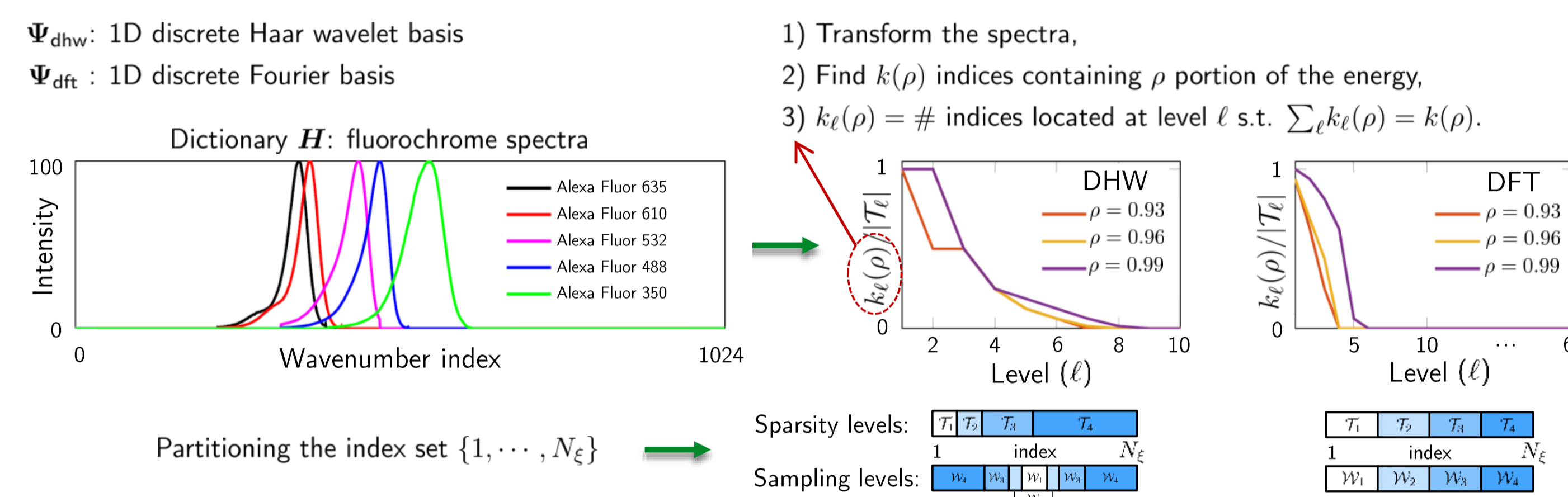


## 4. Coded Illumination-FTI (CI-FT)

- Acquisition model:



- Sparsity in levels in different possible bases  $\Psi$ :



- Optimum coding:

**Initial approach [1]:** application-independent, based on the Variable Density Sampling scheme [2],  
 $\Psi = \Psi_{dhw}$ : select  $M \gtrsim K \log^3(K) \log^2(N_\xi)$  w.r.t.  $\mathbb{P}[\xi \in \Omega] \propto \frac{1}{|\xi - N_\xi/2|}$  (with replacement)

**New approaches:** application-dependent, based on the Multilevel Density Sampling scheme [3],

$\forall$  sampling levels  $t$   
 $\Psi = \Psi_{dhw}$ : select  $m_t \gtrsim \sum_{\ell} 2^{-\frac{t-\ell}{2}} k_\ell \log(K) \log(N_\xi)$  w.r.t.  $\mathbb{P}[\xi \in \Omega \mid \xi \in \mathcal{W}_t] = \frac{m_t}{|\mathcal{W}_t|}$   
 $\Psi = \Psi_{dft}$ : select  $m_t = |\mathcal{W}_t| \delta_{k_t}$  (without replacement)

$K = \sum_t k_t$  and  $M = \sum_t m_t$

- Recovery guarantee: for every pixel  $j = 1, \dots, N_p$ , solve

$$\hat{x}_j = \arg \min_{\mathbf{u} \in \mathbb{C}^N} \|\Psi^T \mathbf{u}\|_1 \text{ s.t. } \|D(\mathbf{y}_j - R_\Omega \Phi_{dft}^* \mathbf{u})\|_2 \leq \varepsilon \sqrt{M} \approx \varepsilon \sqrt{N_\xi}$$

$$\|\mathbf{x} - \hat{\mathbf{x}}\| \lesssim \left( \sum_{j=1}^{N_p} \alpha^2(\Psi^T \mathbf{x}_j) \right)^{1/2} + \varepsilon \sqrt{N_p}$$

**Initial approach:**  $\Psi = \Psi_{dhw}$ ,  $d_{ii} = \mathbb{P}[\Omega_i \in \Omega]^{-1/2}$ ,  $\alpha(\mathbf{u}) = \frac{\|\mathcal{H}_{k_\ell}(\mathbf{u})\|_1}{\sqrt{K}}$  (hard thresholding)

**New approach 1:**  $\Psi = \Psi_{dhw}$ ,  $d_{ii} = N_\xi^{-1/2}$ ,  $\alpha(\mathbf{u}) = \sum_{\ell} \|R_{\mathcal{T}_\ell} \mathbf{u} - \mathcal{H}_{k_\ell}(R_{\mathcal{T}_\ell} \mathbf{u})\|_1$

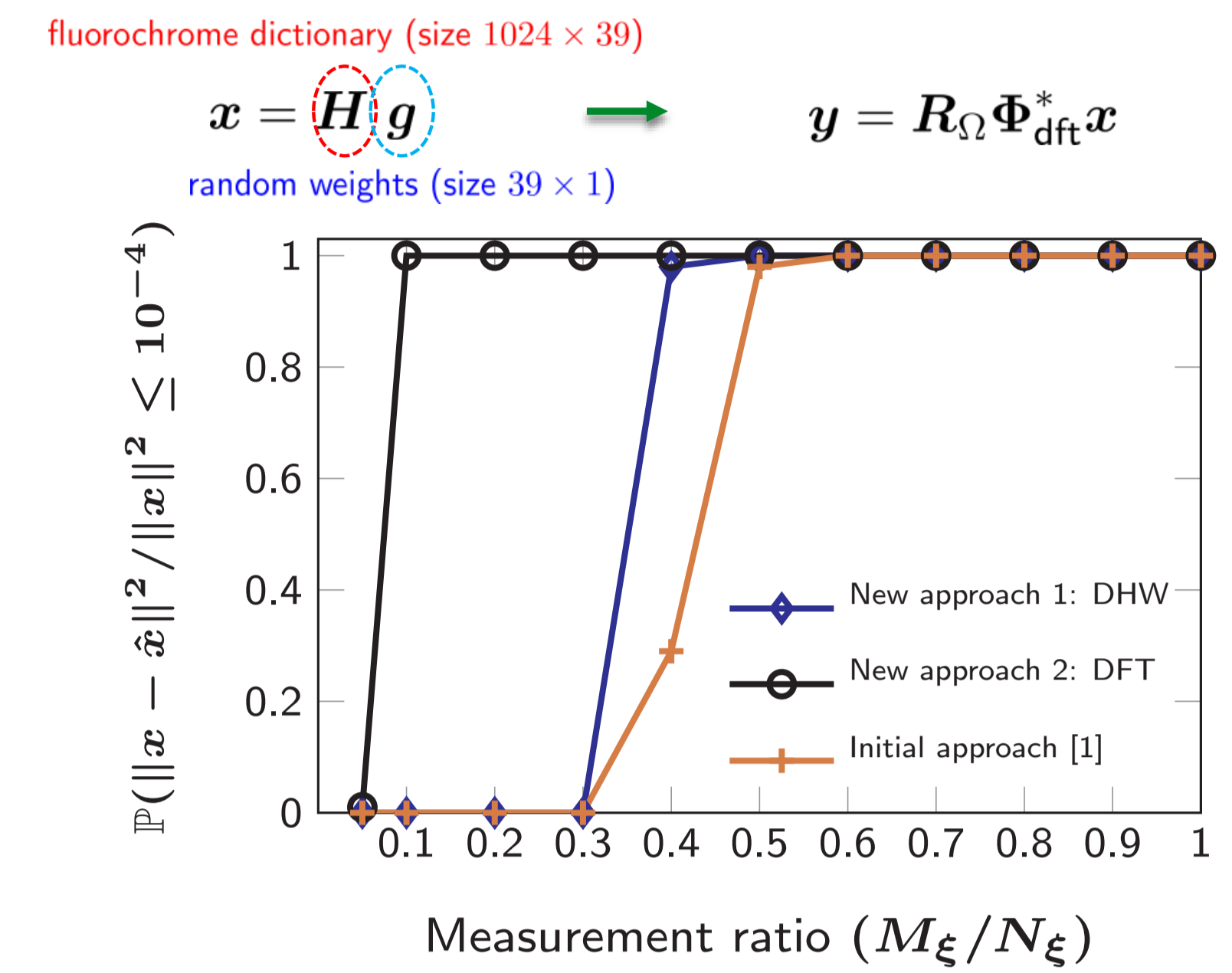
**New approach 2:**  $\Psi = \Psi_{dft}$ ,  $d_{ii} = N_\xi^{-1/2}$ ,  $\alpha(\mathbf{u}) = \sum_{\ell} \|R_{\mathcal{T}_\ell} \mathbf{u} - \mathcal{H}_{k_\ell}(R_{\mathcal{T}_\ell} \mathbf{u})\|_1$

## 7. References

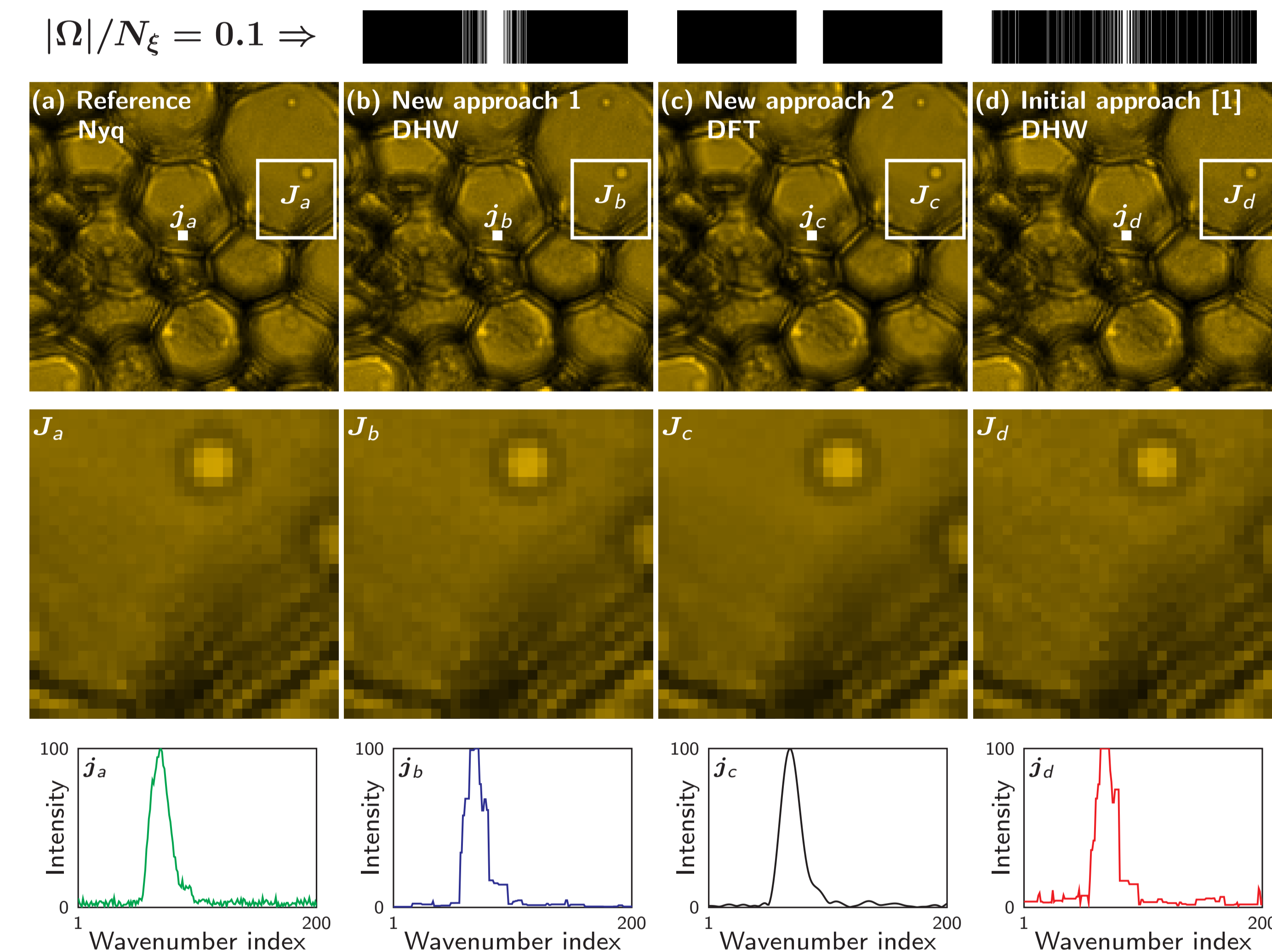
- [1] A. Moshtaghpour, V. Cambareni, P. Antoine, M. Roblin, and L. Jacques, "A variable density sampling scheme for compressive Fourier transform interferometry," arXiv preprint arXiv: 1801.10432v2, 2018.
- [2] F. Kramher and R. Ward, "Stable and robust sampling strategies for compressive imaging," *IEEE Transactions on Imaging Processing*, vol. 23, no. 2, pp. 612–622, 2013.
- [3] B. Adcock, A. C. Hansen, C. Poon, and B. Roman, "Breaking the coherence barrier: A new theory for compressed sensing," *Forum of Mathematics, Sigma*, vol. 5. Cambridge University Press, 2017.

## 5. Numerical Results

- Synthetic measurements: phase transition curves of successful recovery



- Real FTI measurements: comparison of recovery quality



Illumination coding pattern (first row), reconstructed spatial maps at 594 nm wavelength (second and third row), and reconstructed spectra at the center pixel (bottom).

## 6. Take Home Messages

- A non-uniform density sampling must be deployed for coherent sampling/sparsity bases.
- The Variable Density Sampling (VDS) scheme [2] is an application-independent optimum strategy that provides uniform recovery guarantee.
- The Multilevel Density Sampling (MDS) scheme [3] is an application-dependent optimum strategy that provides non-uniform recovery guarantee.
- Both VDS and MDS schemes can be leveraged for the realization of CI-FTI in (less photo-bleaching) fluorescent spectroscopy.
- MDS scheme results in superior reconstruction as it takes into account the sparsity structure of the fluorochrome spectra.